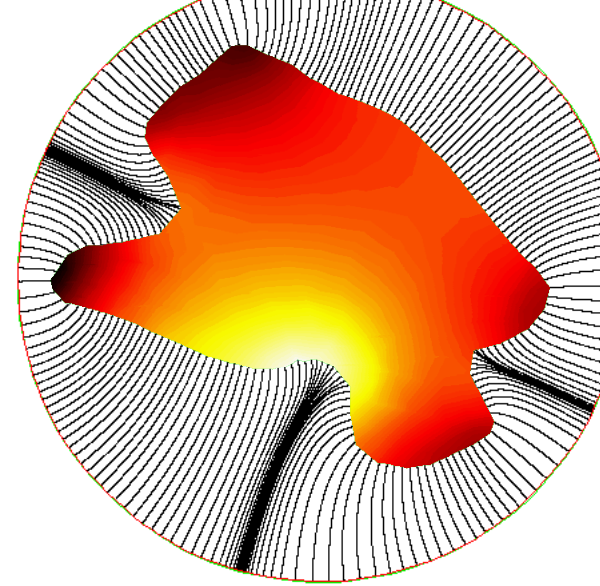


# Mapping amoeboid cell migration

Till Bretschneider  
Warwick Systems Biology Centre



InnoMol BiImaging workshop 22<sup>nd</sup> October 2014, Ruđer Bošković Institute,  
Zagreb

THE UNIVERSITY OF  
**WARWICK**

# Outline

## Part I: Methods (LineageTracker, CellTracker, QuimP)

- Introduction to graph based approaches for multi cell (point) tracking and image segmentation
- Surface matching: Tackling biological shape variability (active contour based methods)
- Utilising inexpensive GPU computing for fast 3D real time imaging of Light Sheet Microscopy Data

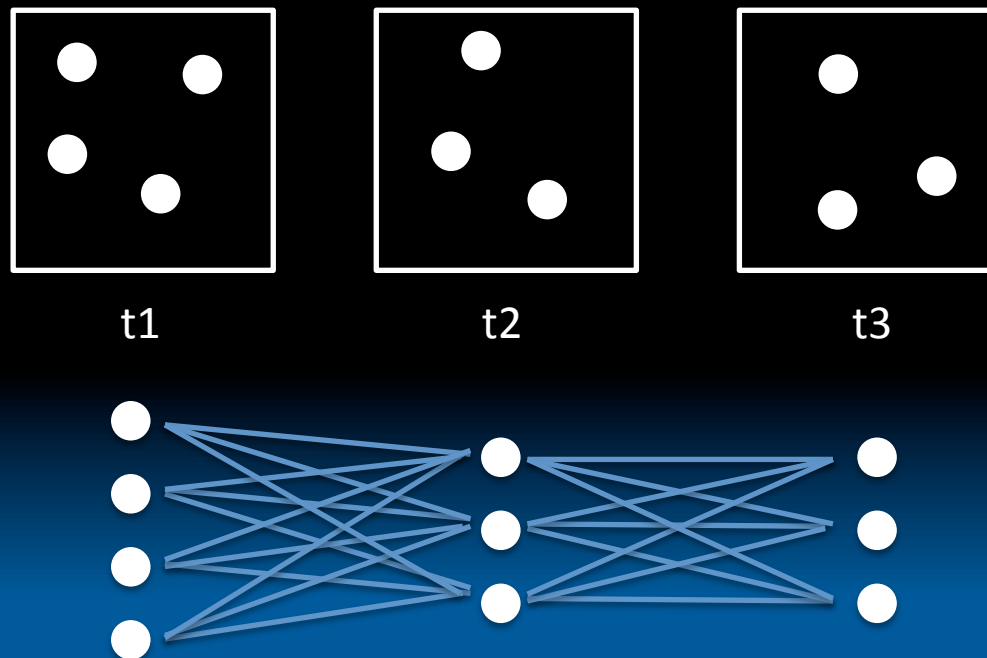
## Part II: Applications: Tracking spatio-temporal fluorescence distributions in migrating cells

- Biochemistry: Fitting mathematical models for cell reorientation to time series image data
- Cellular Mechanics: Blebbing
  - Zatulovskiy E, Tyson R, Bretschneider T, Kay RR. Bleb-driven chemotaxis of Dictyostelium cells. J Cell Biol. 2014 Mar 17;204(6):1027-44.
  - Tyson RA, Zatulovskiy E, Kay RR, Bretschneider T. How blebs and pseudopods cooperate during chemotaxis. Proc Natl Acad Sci U S A. 2014 Aug 12;111(32):11703-

# Cell tracking using multi feature global optimisation

- LineageTracker: ERASysBio project to investigate the connection between the cell cycle and the clock using FUCCI markers (tracking cell nuclei)

Feillet C, Krusche P, Tamanini F, Janssens RC, Downey MJ, Martin P, Teboul M, Saito S, Lévi FA, Bretschneider T, van der Horst GT, Delaunay F, Rand DA. Phase locking and multiple oscillating attractors for the coupled mammalian clock and cell cycle. Proc Natl Acad Sci U S A. 2014 Jul 8;111(27):9828-33.



Graph: consists of nodes (vertices) and edges

Weight matrix  $W$ : edges weighted according to similarity of nodes

	+1	+2	e	f	g
a			$w_{ae}$	$w_{af}$	$w_{ag}$
b			$w_{be}$	$w_{bf}$	$w_{bg}$
c			$w_{ce}$	$w_{cf}$	$w_{cg}$
d			$w_{de}$	$w_{df}$	$w_{dg}$

Similarity (weight) matrix can account for multiple features:

- distance of cells
- differences in brightness, area, shape
- cell state (dividing, post division)
- multiple channel information ...

Weights describe the probability  $P$  that two cells at subsequent time points are identical.

$P$  can be converted into a cost ( $1-P$ ). Standard methods from linear algebra for minimising the total cost exist (Hungarian algorithm and derivatives)

Adjacency matrix A captures the structure of the graph

Diagram showing a graph with 5 nodes (1, 2, 3, 4, 5) and 4 edges (a, b, c, d). The edges connect nodes 1-2 (a), 2-3 (b), 3-4 (c), and 4-5 (d).

		nodes				
		①	②	③	④	⑤
edges	a	-1	1	0	0	0
	b	0	-1	1	0	0
	c	0	0	-1	1	0
	d	0	0	0	-1	1

Constitutive matrix C containing weights for each edge

	a	b	c	d
a	$w_a$	0	0	0
b	0	$w_b$	0	0
c	0	0	$w_c$	0
d	0	0	0	$w_d$

The graph Laplacian matrix  $L=A^TCA$  incorporates both, the structure and weights

L is the discrete version of the continuous Laplace operator

$$L = \text{div grad} = \delta^2/\delta x^2$$

# Random walks for image segmentation

Graph Laplacian  $L = \text{div grad} = \delta^2/\delta x^2$

L is associated with diffusion problems or random walks.

Fick's 2<sup>nd</sup> law of diffusion:  $\delta u/\delta t = D \delta u^2/\delta x^2$

u: concentration, electric potential, temperature, image brightness

Laplace's equation:  $\delta u^2/\delta x^2 = 0$  (stationary)

Laplace's equation can be solved by minimizing the Dirichlet integral (potential energy). In effect, diffusion smoothens out all gradients.

Dirichlet integral

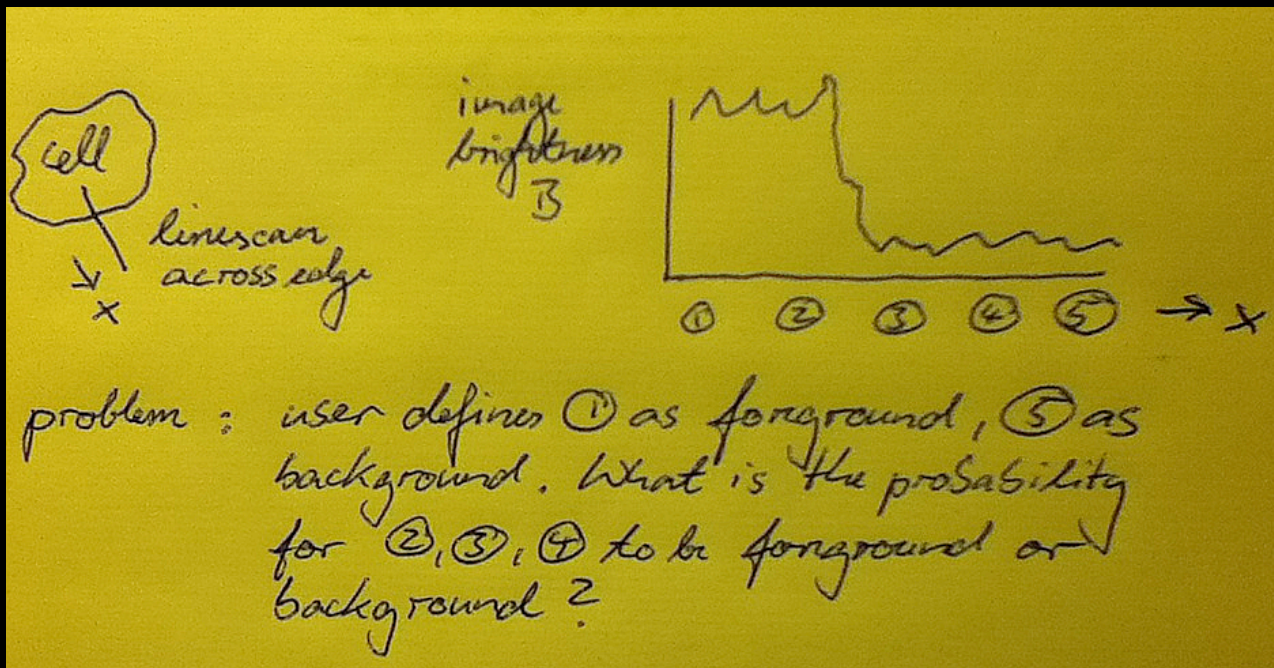
$$D[u] = \frac{1}{2} \int_{\Omega} |\nabla u|^2 d\Omega \quad \text{where } \nabla = \text{grad}$$

The corresponding problem on a graph is solved by finding:

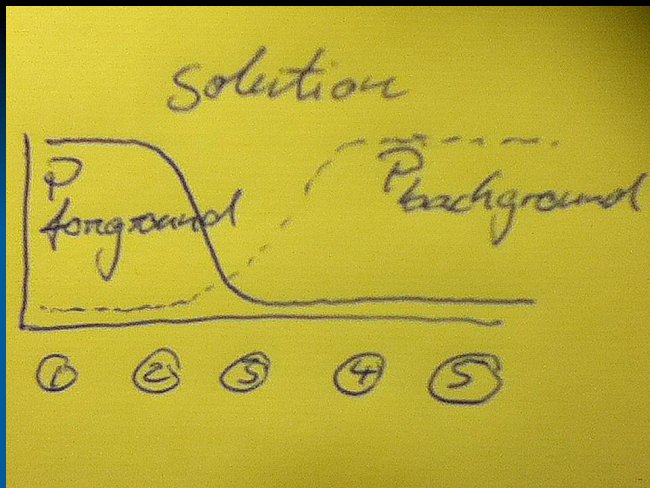
$$\min \frac{1}{2} u^T L u = \frac{1}{2} \sum |u_i - u_j|^2$$

with suitable boundary conditions

# Supervised segmentation: user provide boundary conditions (partitioning of a graph)



Consider diffusion on the graph with node 1 as source and node 5 as sink. Diffusion is limited across edges with low similarity, ie where we have steps in the image. Anisotropic diffusion preserves edges.



$P_{\text{fg}} > P_{\text{bg}}$  : assign pixel to foreground

$P_{\text{bg}} > P_{\text{fg}}$  : assign pixel to background

Probabilistic framework allows to put confidence limits on segmentation, for example to restrict processing to regions of high confidence

## Advantages of the random walk segmentation (and its many variants)

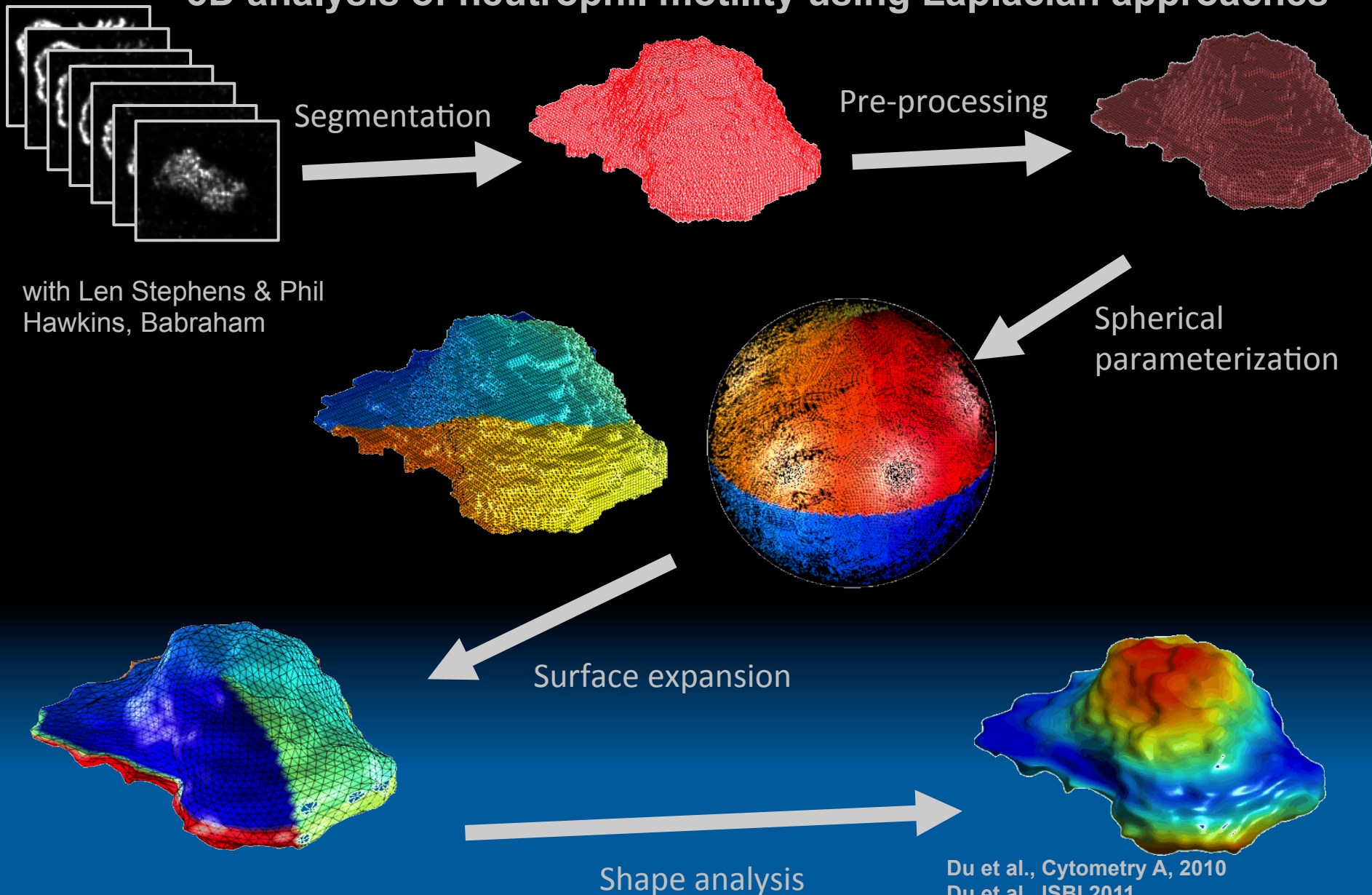
- Multi object segmentation possible (cell cluster)
- Enables neutral segmentation (separating cells with identical intensities)
- Works in 3D
- Multiple features can be integrated (intensity, texture, multiple colour channels, ...)
- Computationally very efficient
- Sound theoretical basis

## CellTracker software: Measuring nucleus-cytoplasmic translocations of transcription factors

Xue M, Momiji H, Rabbani N, Barker G, Bretschneider T, Shmygol A, Rand D, Thornalley PJ. Frequency modulated translocational oscillations of Nrf2 mediate the ARE cytoprotective transcriptional response. *Antioxid Redox Signal*. 2014 Sep 2. [Epub ahead of print]



# 3D analysis of neutrophil motility using Laplacian approaches

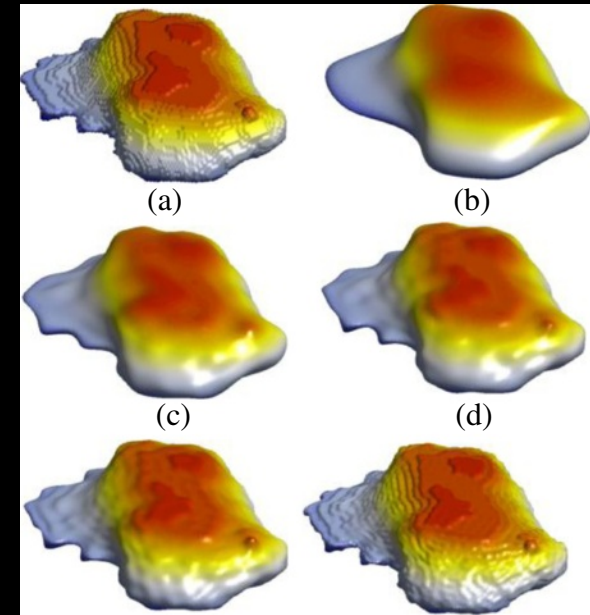


Du et al., Cytometry A, 2010  
Du et al., ISBI 2011  
Du et al., ISBI 2012  
Du et al., BMVC 2012  
Du et al., BMC Bioinformatics, 2013

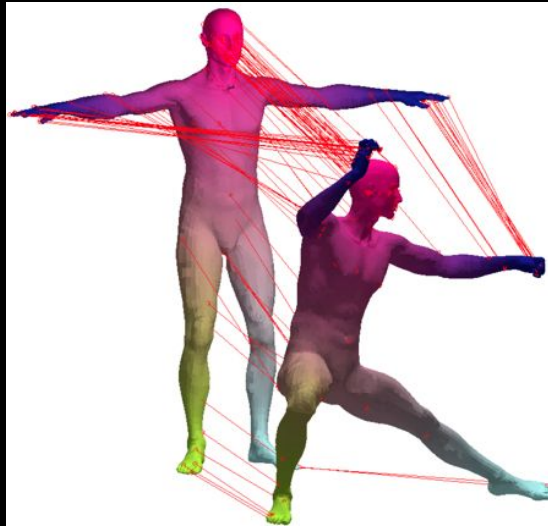
## Quantifying shape deformations

Problem: find corresponding nodes on two surface meshes

- Rigid transformations
- Using fiducial markers
- 3D shape matching using spherical parameterisation
- Direct feature matching (curvature/intensity, ...) using spectral coordinates (modes/eigenvectors of the graph Laplacian) to constrain the problem (regularisation)
- Deformable contours/surfaces (QuimP)



# Spectral alignment methods



## **FOCUSR: Feature Oriented Correspondence Using Spectral Regularization--A Method for Precise Surface Matching**

Herve Lombaert, Leo Grady, Jonathan R. Polimeni, Farida Cheriet  
*Pattern Analysis and Machine Intelligence, IEEE Transactions on* , vol.35, no.9, pp.  
2143,2160, Sept. 2013

Eigendecomposition of the graph Laplacian matrix its eigenmodes (eigenvectors) reveals strong correspondences between shapes

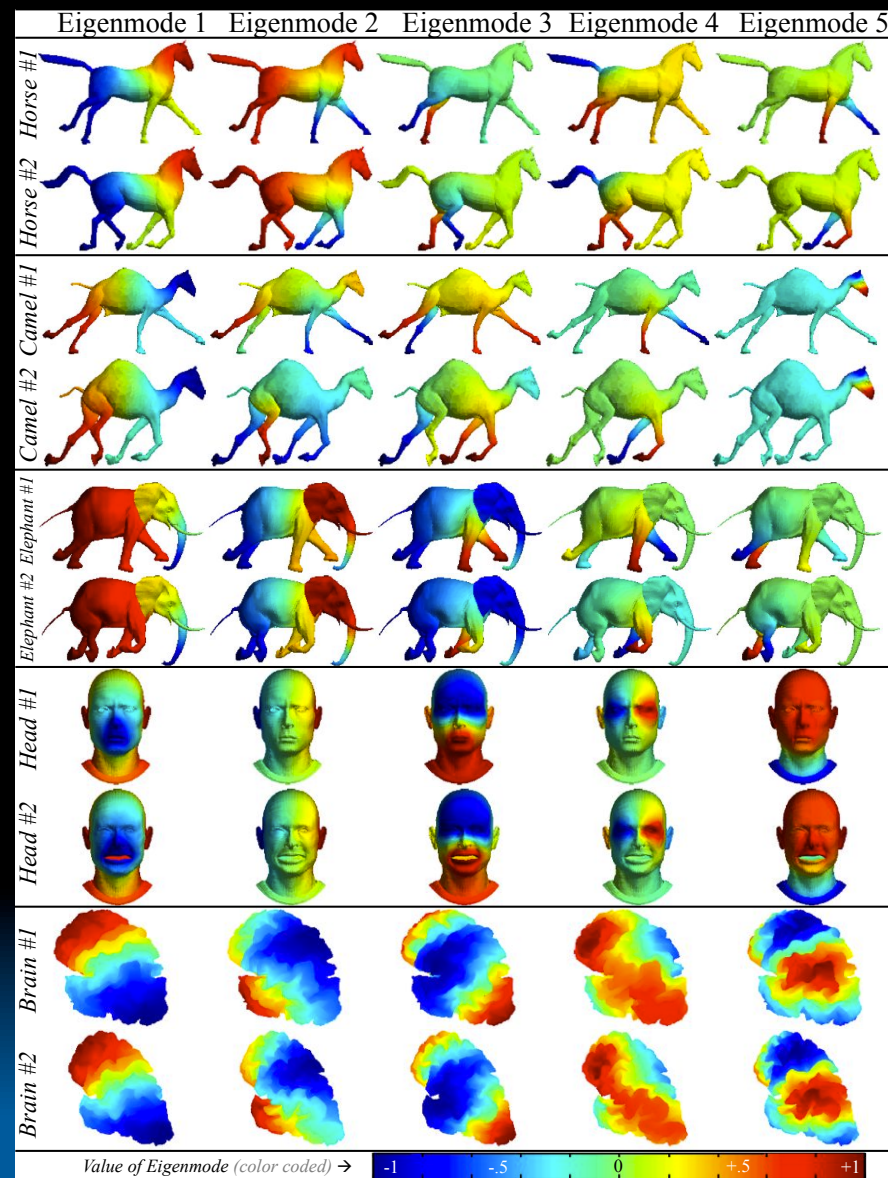
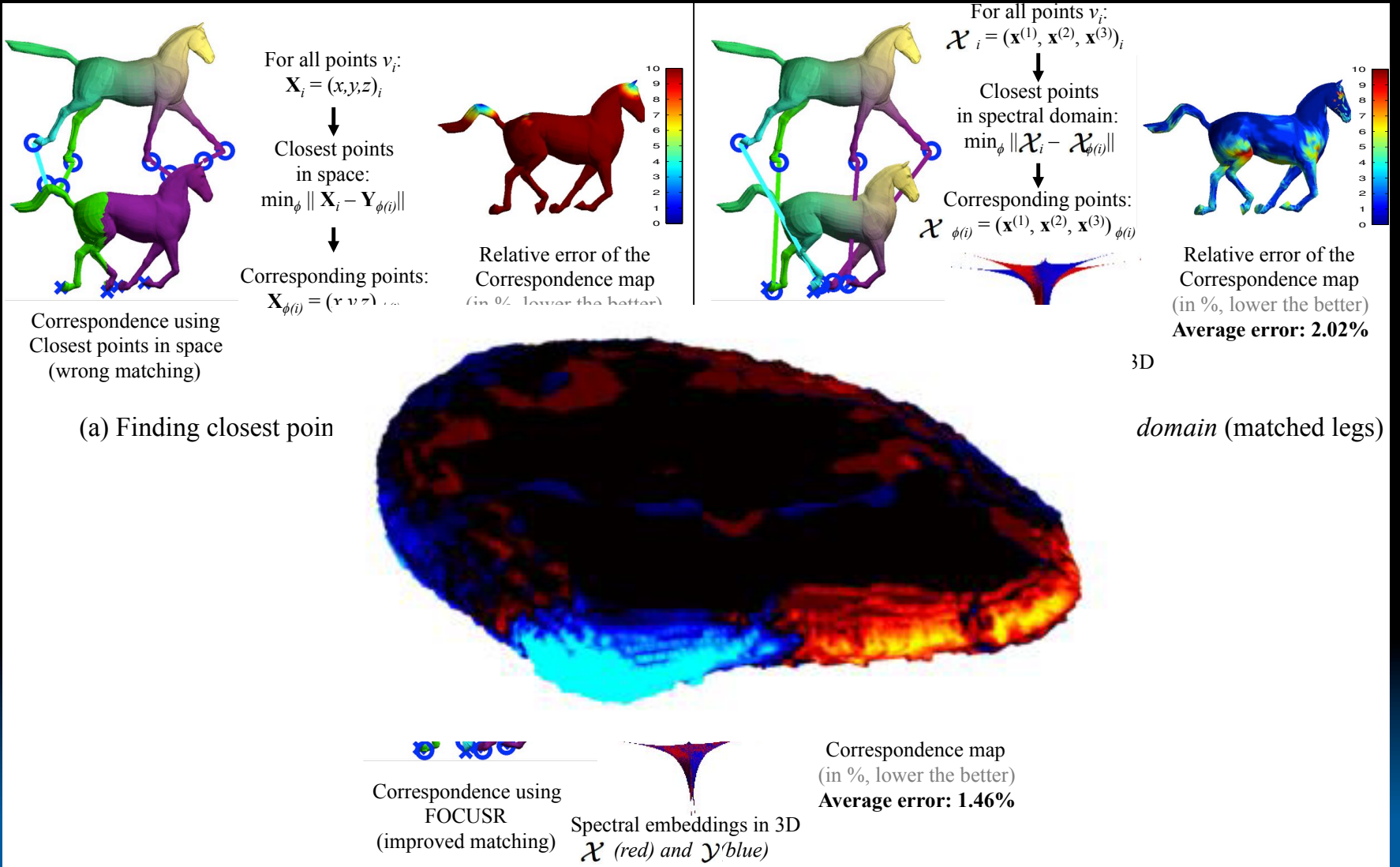
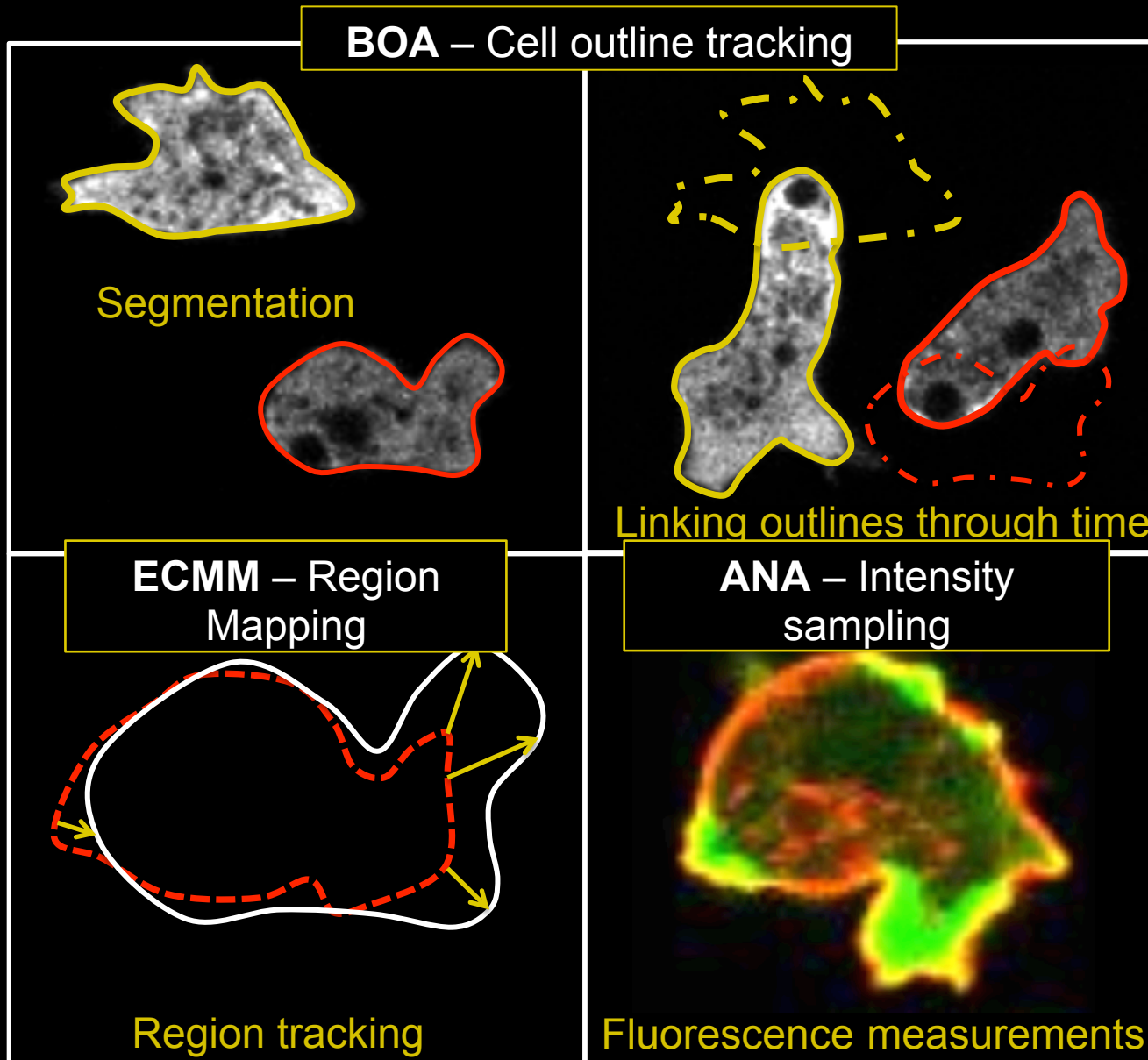


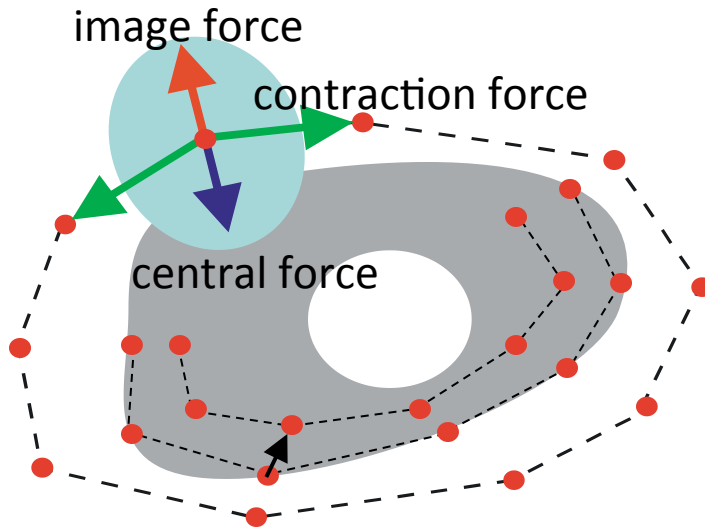
Fig. 1. Example of eigenmodes for pairs of animals and human brain surfaces. Each row shows the first five spectral components of a model (eigenmodes of the associated graph Laplacian, reordered and sign adjusted, so paired sets match). The color scale indicates the value of the spectral coordinate over the surface.



# QuimP: ImageJ plugins for quantifying cellular morphodynamics



# Active contour based methods for automated cell outline detection



$$\vec{F}_i = Z * \vec{F}_i^{central} \cdot K * \vec{F}_i^{contraction} \cdot B * \Delta h_i \vec{F}_i^{image} \cdot \vec{F}_i^{friction} \quad (1)$$

$$m * \dot{\vec{v}}_i^t = \vec{F}_i \quad (2)$$

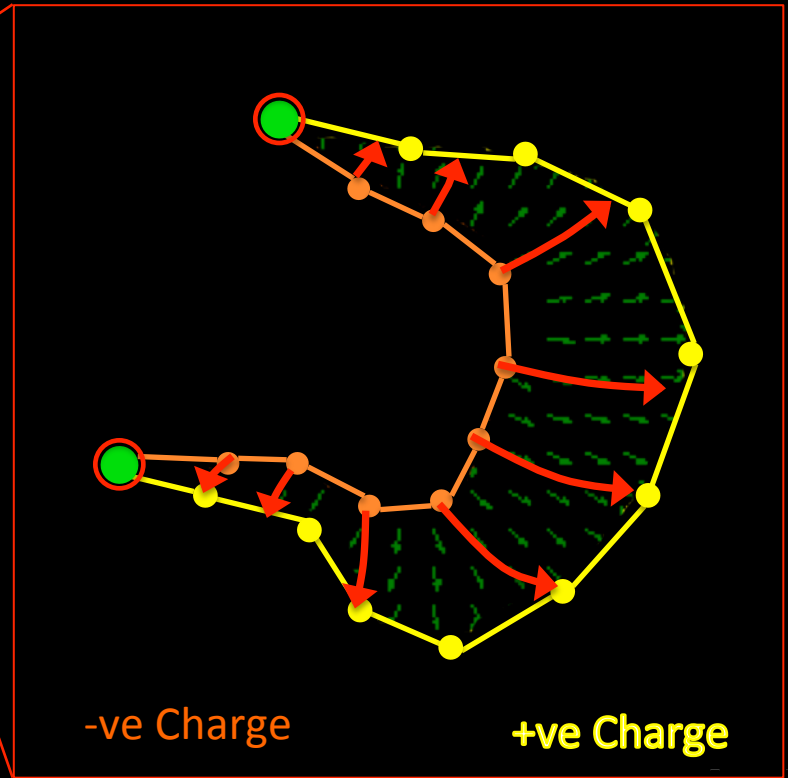
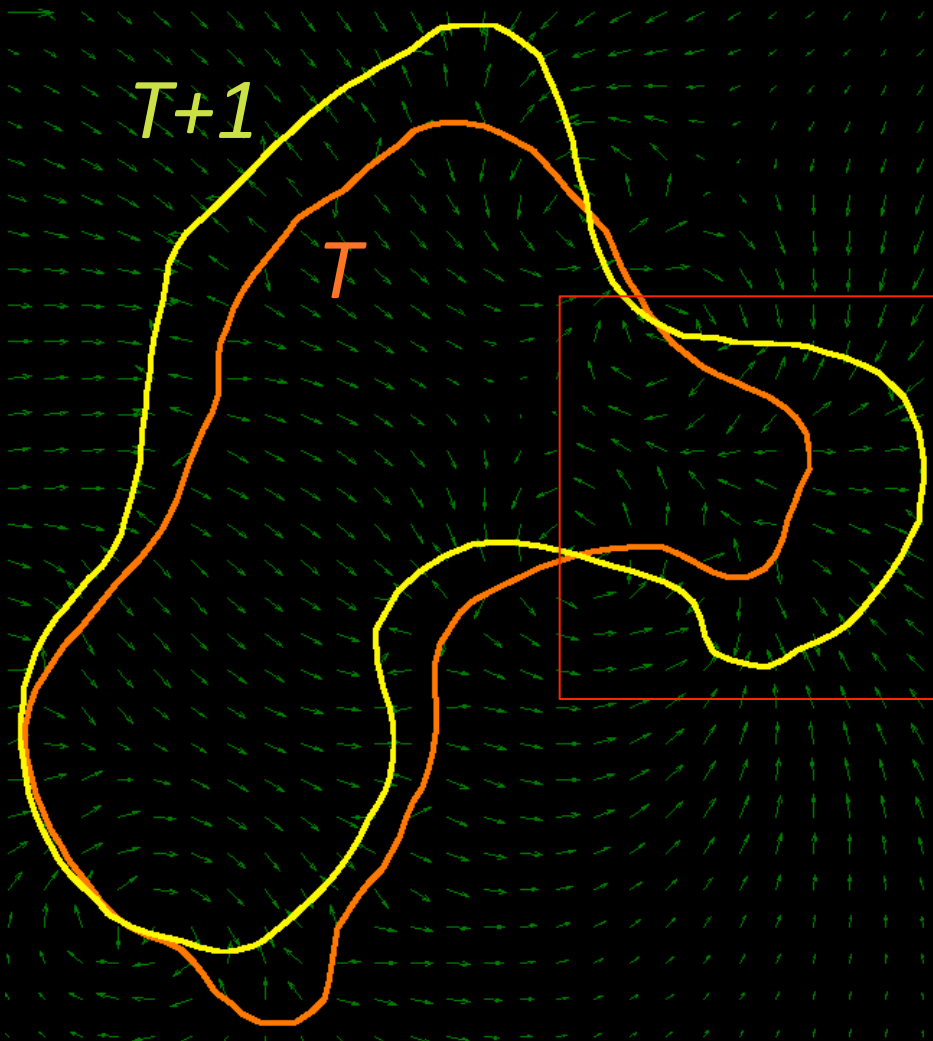
$$\vec{v}_i^t \cdot dt = \vec{v}_i^t \cdot \vec{F}_i^t * dt \quad (3)$$

$$\vec{x}_i^t \cdot dt = \vec{x}_i^t \cdot \vec{v}_i^t \cdot dt * dt \quad (4)$$

The truncation criterion is fulfilled, when  $\vec{v}_i^t < trunc$ .

# Electrostatic Contour Mapping Method

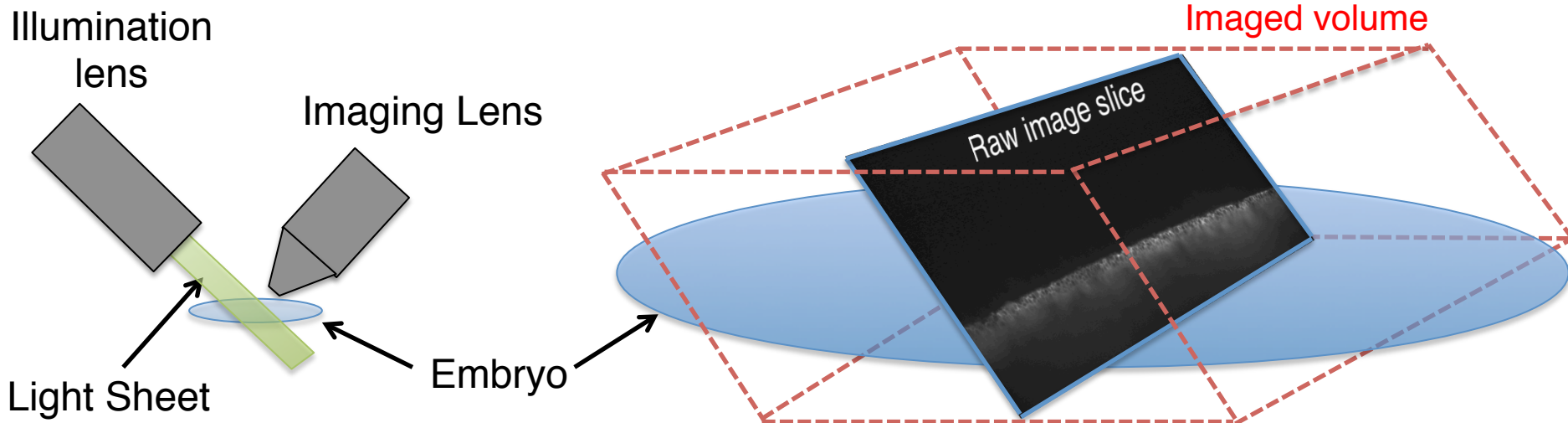
Tyson et al.: High Resolution Tracking of Cell Membrane Dynamics in Moving Cells  
Math. Model. Nat. Phenom. Vol. 5, No. 1, 2010



Field lines do not cross



# Light Sheet Fluorescence Microscopy

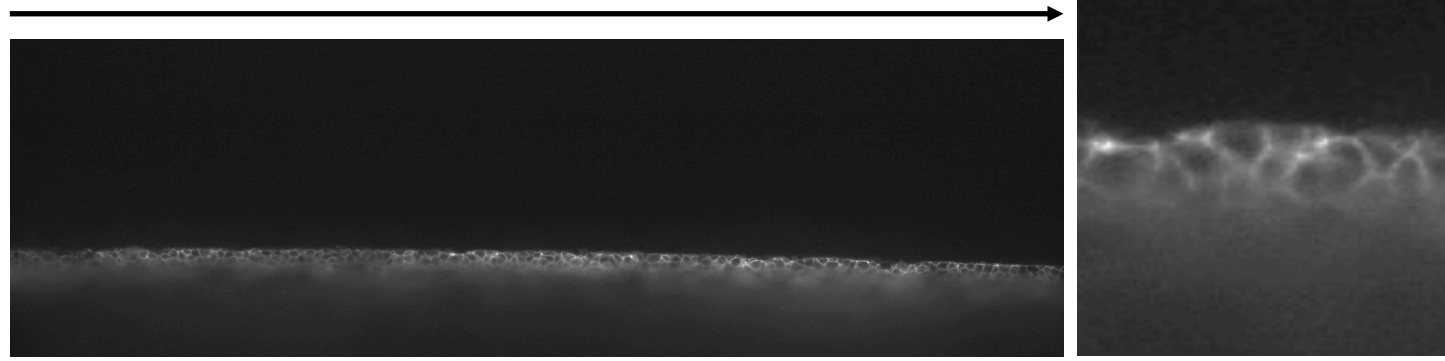


188 sec frame interval  
(~12 hour imaging time)

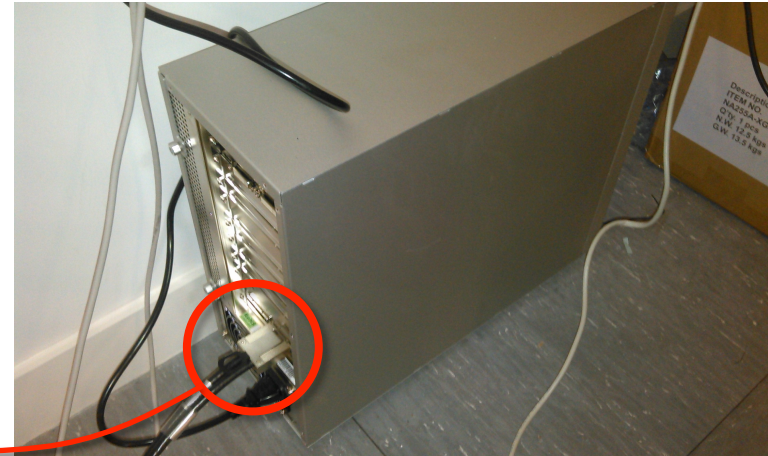
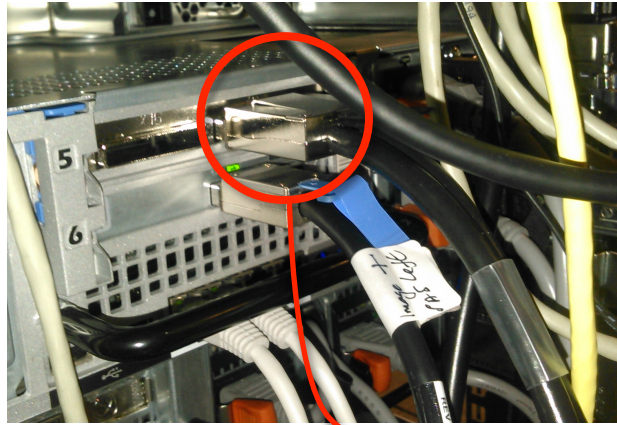
**z - stacking**  
(~2700 slices, 2.6 micron spacing)

2560 pixels (0.65 microns per pixel)

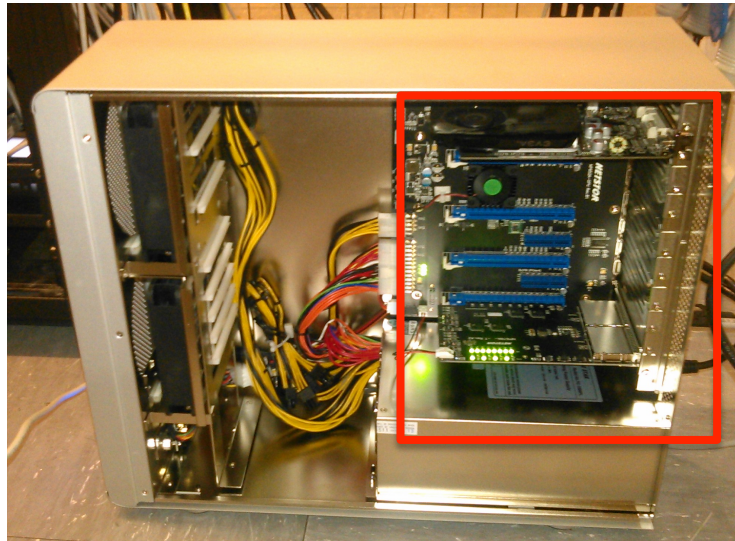
400 pixels  
(0.46 microns per pixel)



# Adding GPU capabilities – Netstore NA255A



PCI express 3.0



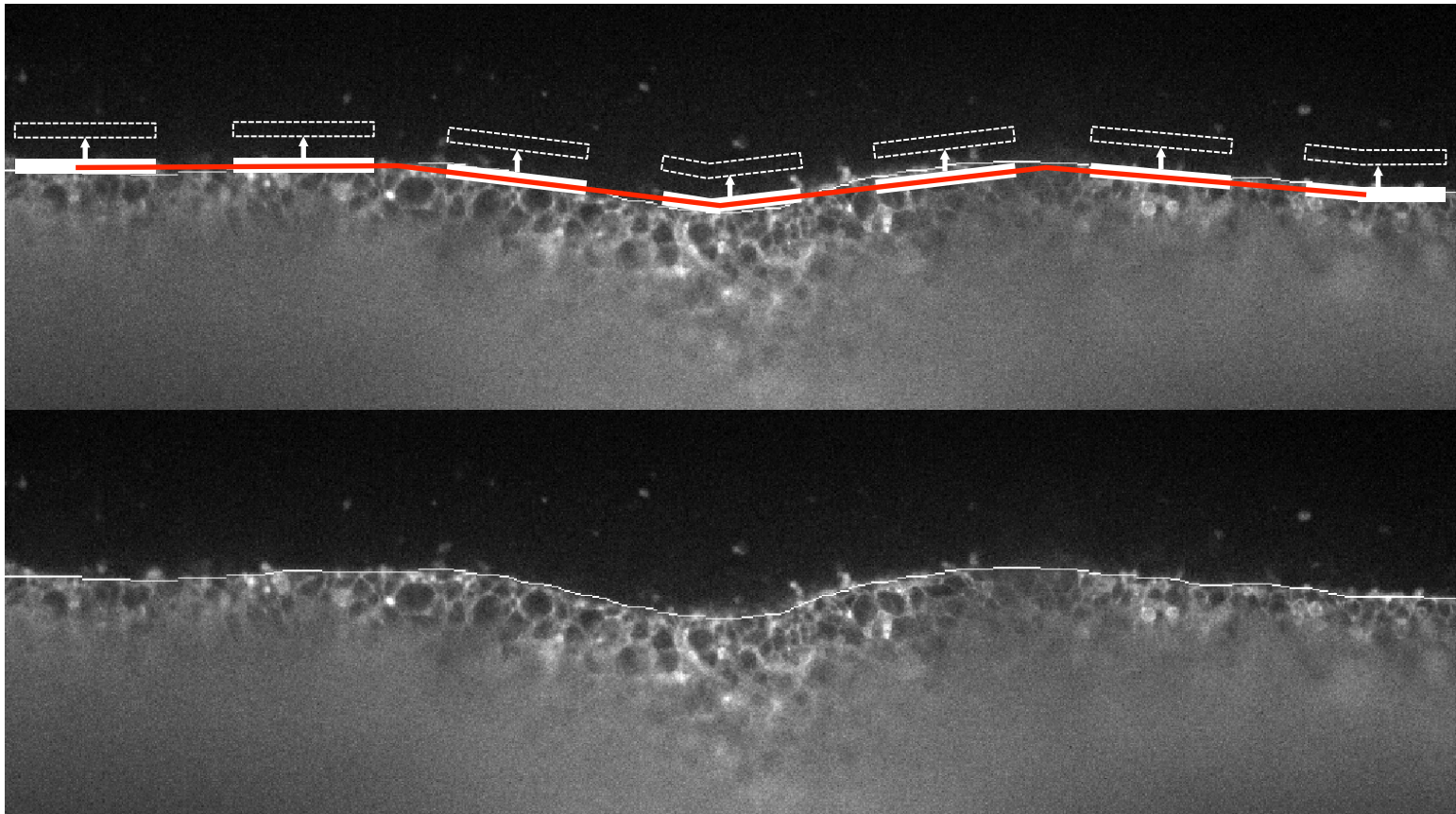
4 GPUs share  
bandwidth  $\approx$  16,000  
MB/s (16 GB/s)

Available to all remote  
users

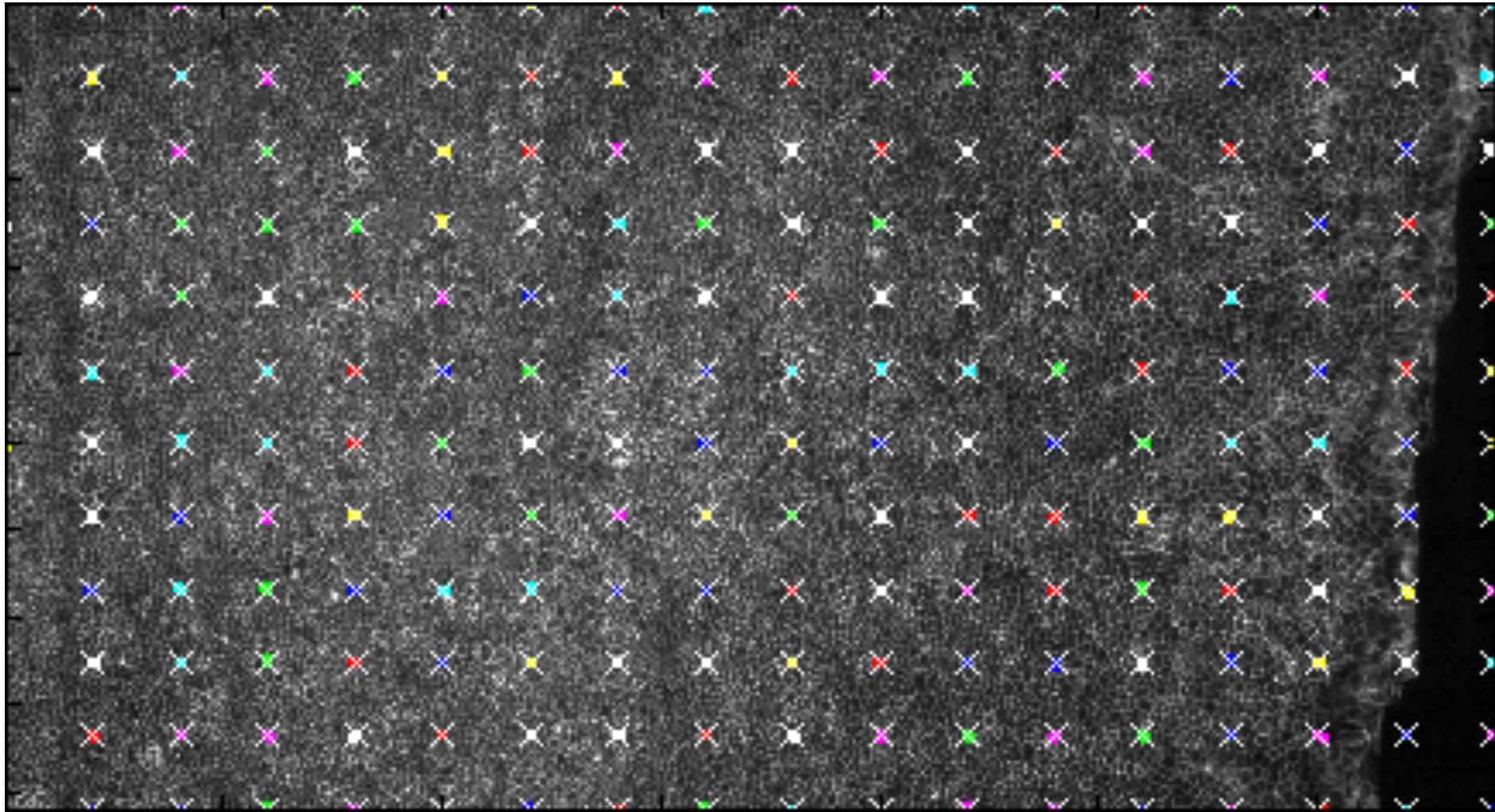
# Surface detection



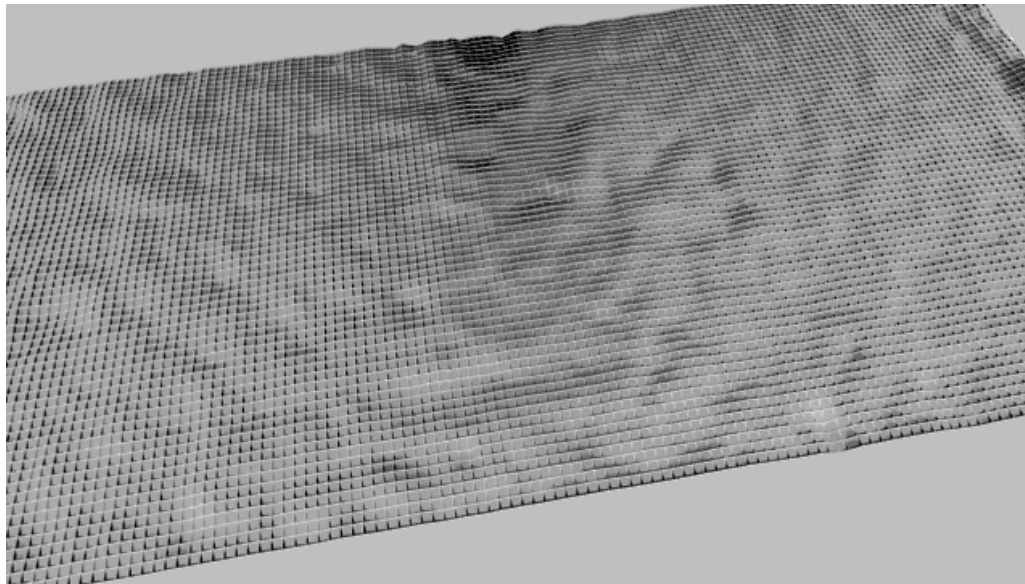
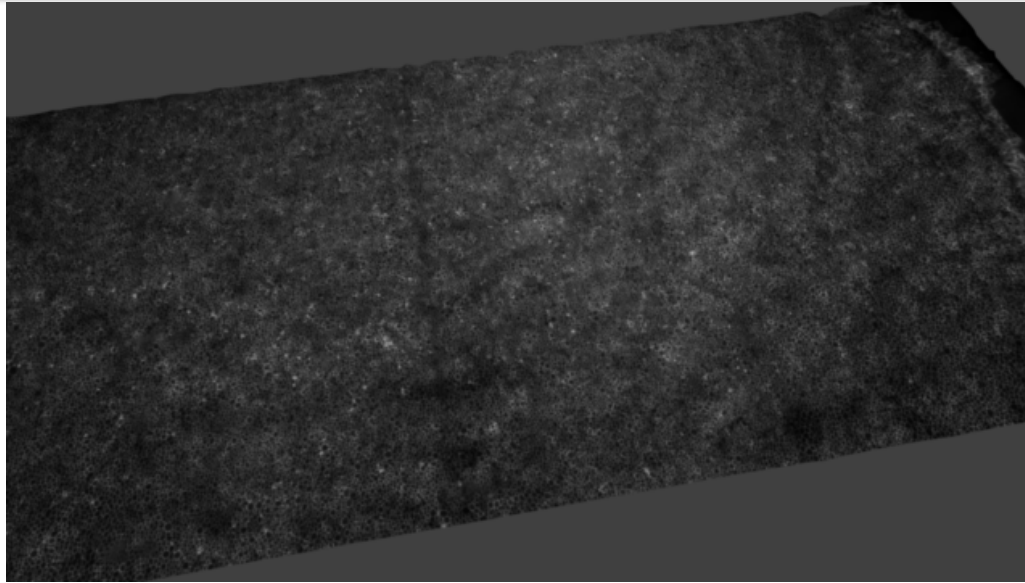
Iteratively warp sampling windows to the surface. Score intensity, variance, and 'sharpness' (via FFT transform)



# Flow analysis using local registration



# 3D visualisation

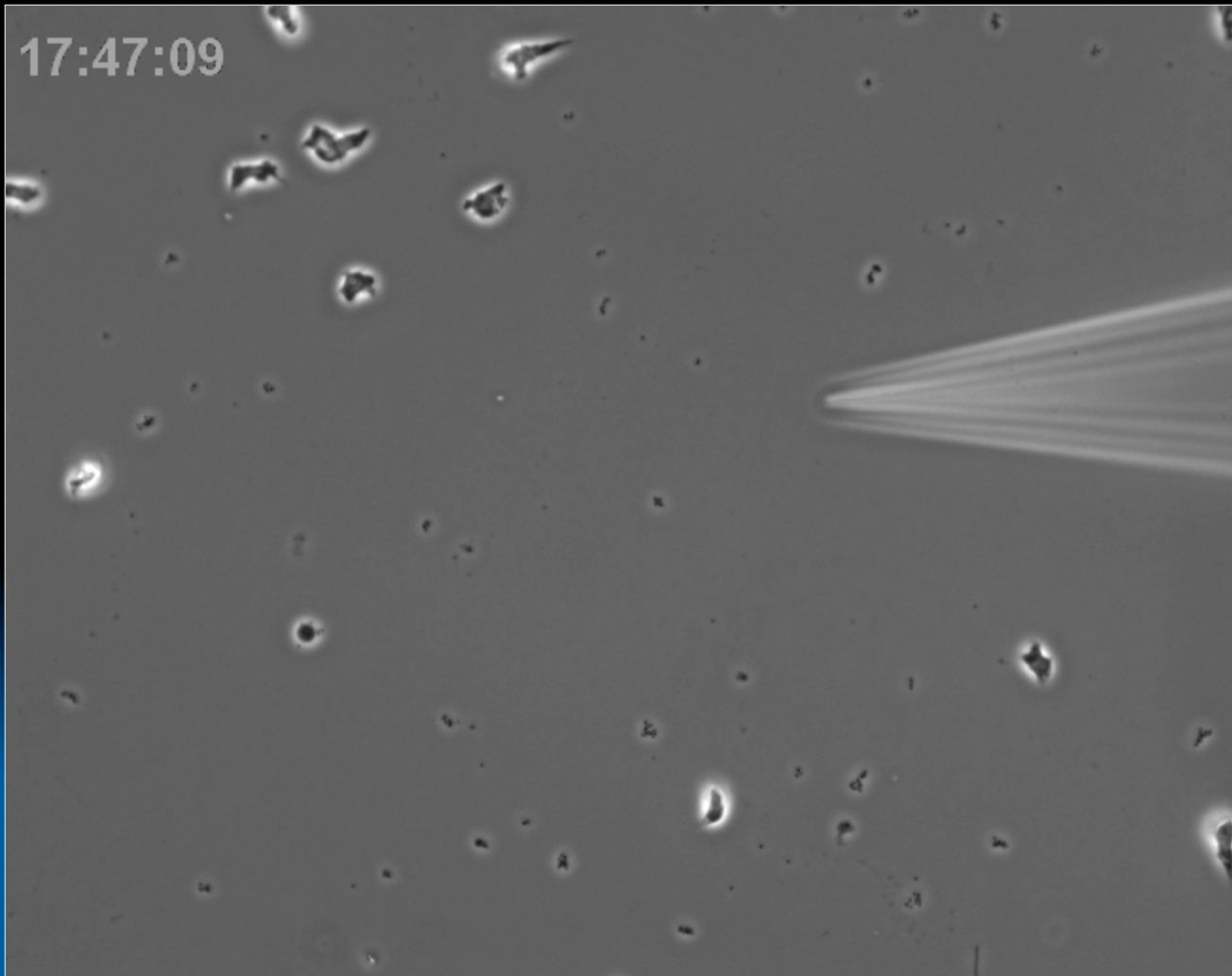


# Real Time Tracking





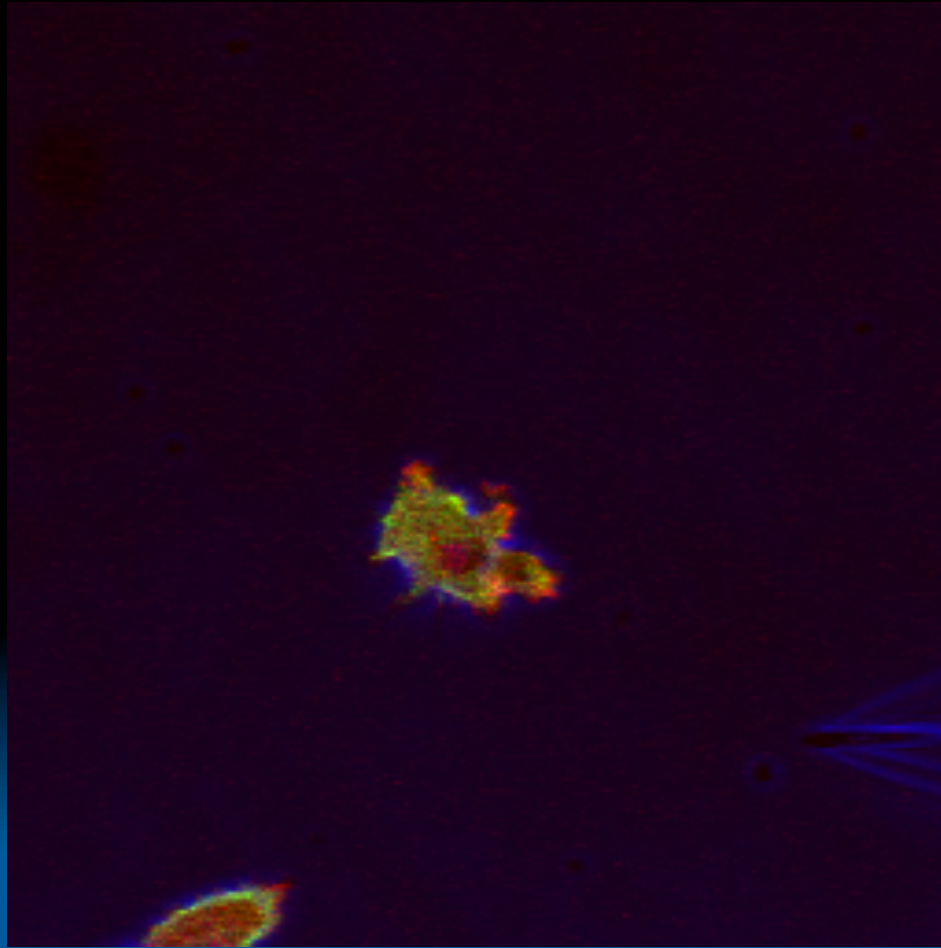
*Dictyostelium*:  
Chemotaxis towards cAMP



(Hans Faix)



# *Dictyostelium* Chemotaxis: Actin-Assembly at the Front and Myosin-II Recruitment to the Tail



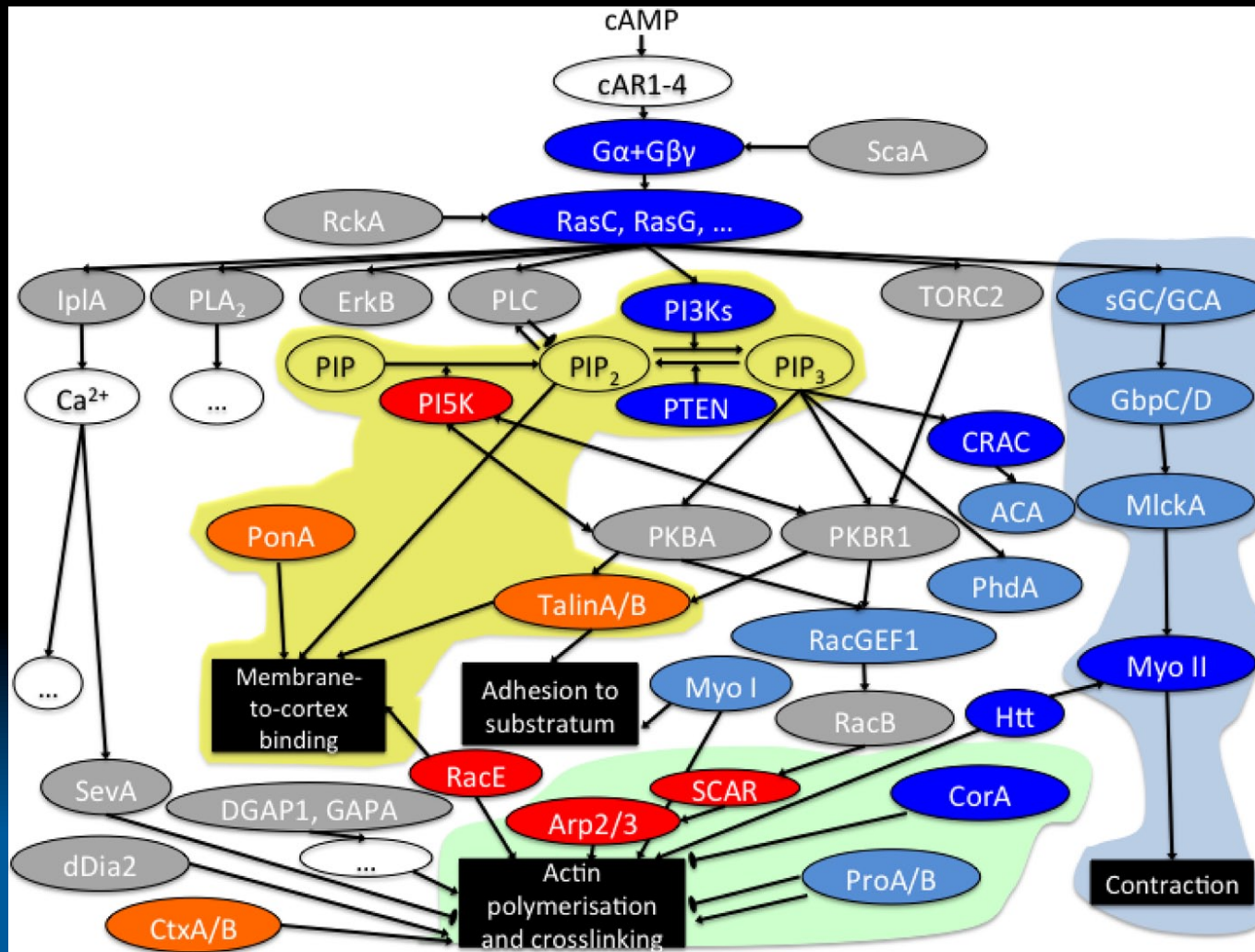
Red: Polymerized actin  
(mRFP-LimE  $\Delta$  coil probe)

Green: Myosin II  
(GFP – heavy chain)

Frame interval: 5 seconds

movie by J. Dalous

# Regulation of Actin polymerization at the front and Myosin-II contraction at the rear



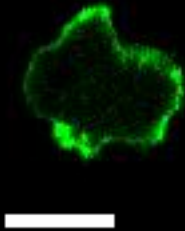
# Questions

How can we extract quantitative data of complex spatio-temporal dynamics?

Can we use mathematical modelling to understand the most basic circuitry underpinning cell polarisation?

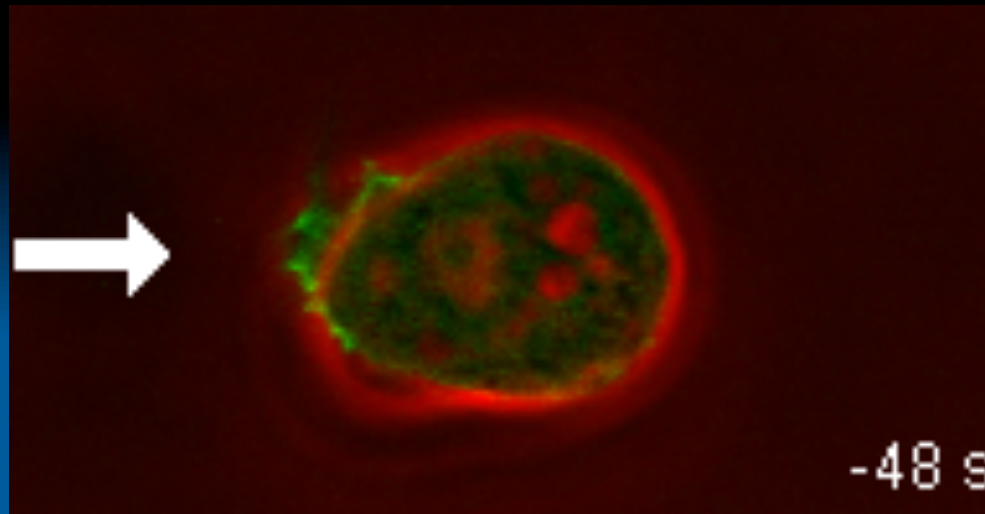
Do unique solutions exist for a particular model?

# Response of *Dictyostelium* to shear flow



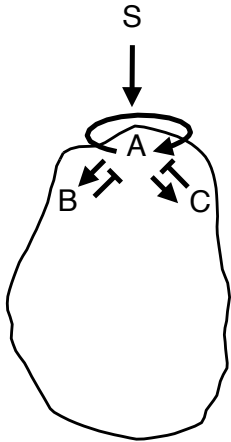
Ingrid Tigges, Warwick

## Polarity reversal at high shear-stresses (2.1 Pa)

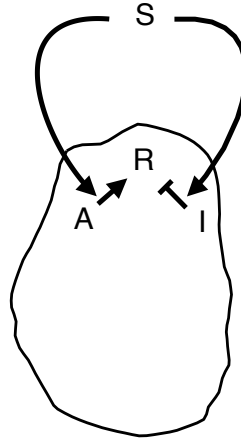


green: Actin label  
red: phase contrast

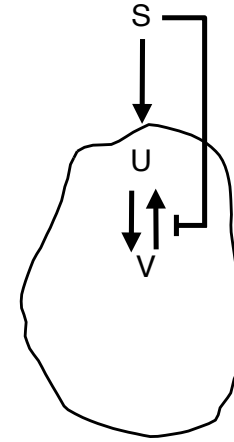
Meinhardt



Levchenko/Iglesias



Otsuji



$$\frac{\partial A}{\partial t} = \frac{sr_a(\frac{A^2}{B} + b_a)}{(s_c + C)(1 + s_a A^2)} - r_a A + D_A \frac{\partial^2 A}{\partial x^2}$$

$$\frac{dB}{dt} = r_b \sum_n \frac{A}{n} - r_b B$$

$$\frac{\partial C}{\partial t} = b_c A - r_c C + D_C \frac{\partial^2 C}{\partial x^2}$$

$$\frac{\partial A}{\partial t} = k_{AS} - k_{-AA} A$$

$$\frac{\partial I}{\partial t} = k_{IS} - k_{-II} I + D \frac{\partial^2 I}{\partial x^2}$$

$$\frac{\partial R}{\partial t} = k_{RA}(R_T - R) - k_{-RI} R$$

$$\frac{\partial U}{\partial t} = a_1 \left[ V - \frac{U + V}{(a_2 s(U + V) + 1)^2} \right] + D_u \frac{\partial^2 U}{\partial x^2}$$

$$\frac{\partial V}{\partial t} = a_1 \left[ \frac{U + V}{(a_2 s(U + V) + 1)^2} - v \right] + D_v \frac{\partial^2 V}{\partial x^2}$$

$$s = (1 + dy \cos(2\pi x))$$

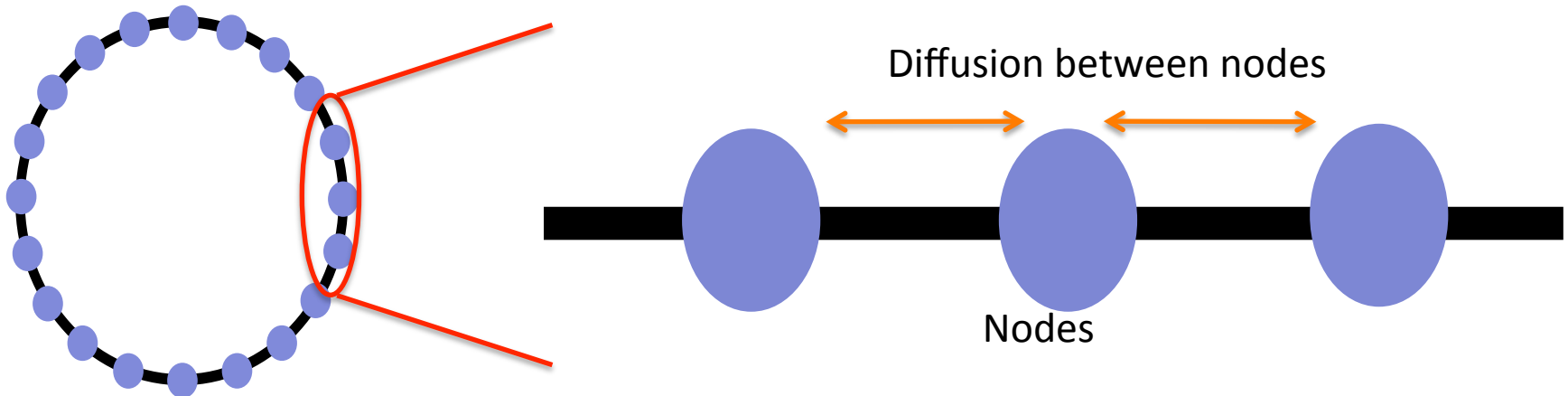
s: external signal, dy is a free parameter to start with

# Model Fitting

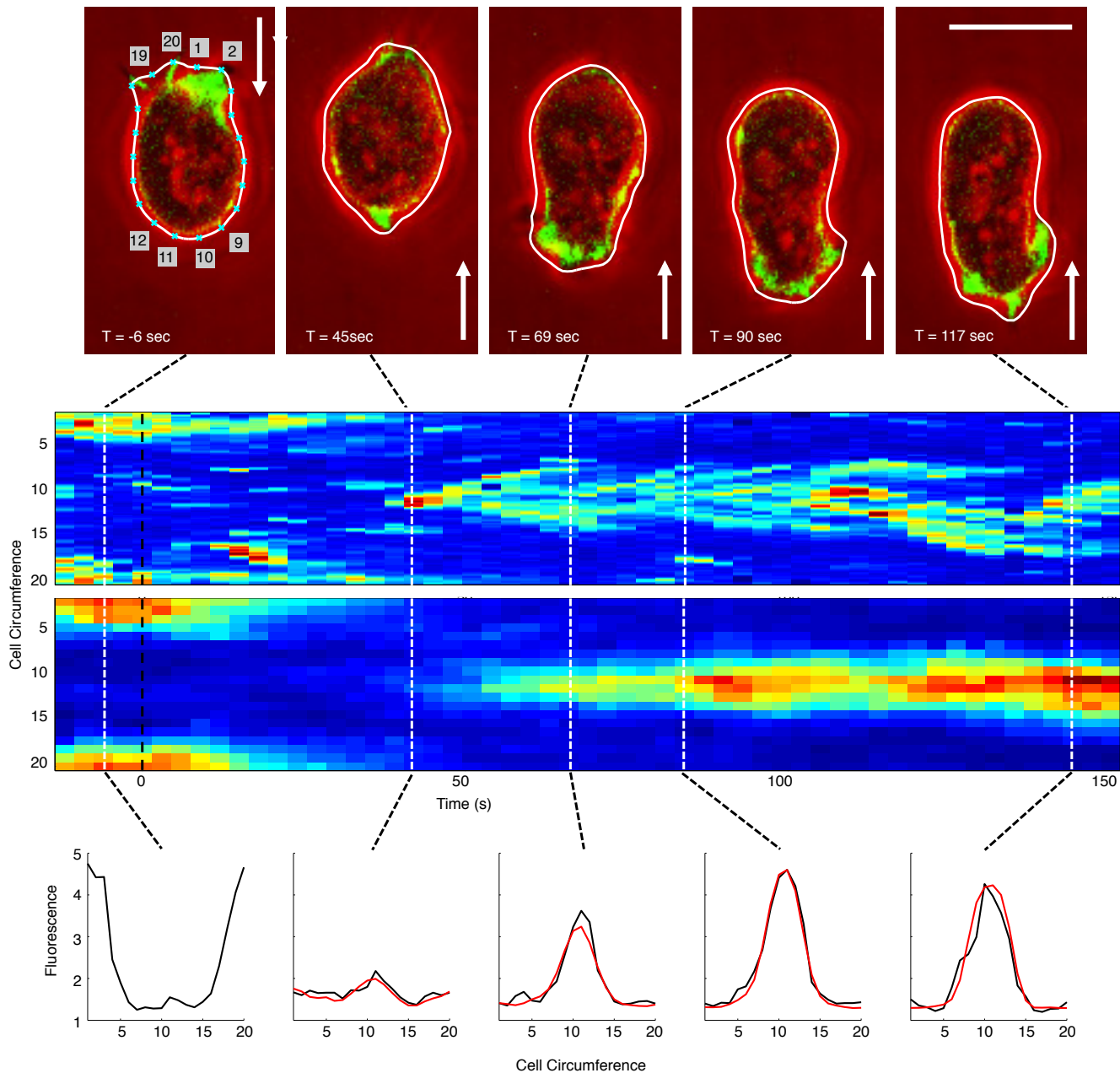
- Implementation in PottersWheel (MATLAB)
- Experimental data: Activator variable resembles actin fluorescence sampled at P=20 points in the cell cortex
- 1D PDE model on a closed circle (periodic boundary conditions)
- Finite difference discretization

$$\partial^2 C_i / \partial x^2 \approx (C_{i-1} - 2C_i + C_{i+1}) / (\Delta x)^2$$

- N-variable PDE problem is expressed as system of P x N ODEs
- Standard ODE solvers (RK45) and NLLS methods (Gauss Newton Trust-region) for fitting can be used

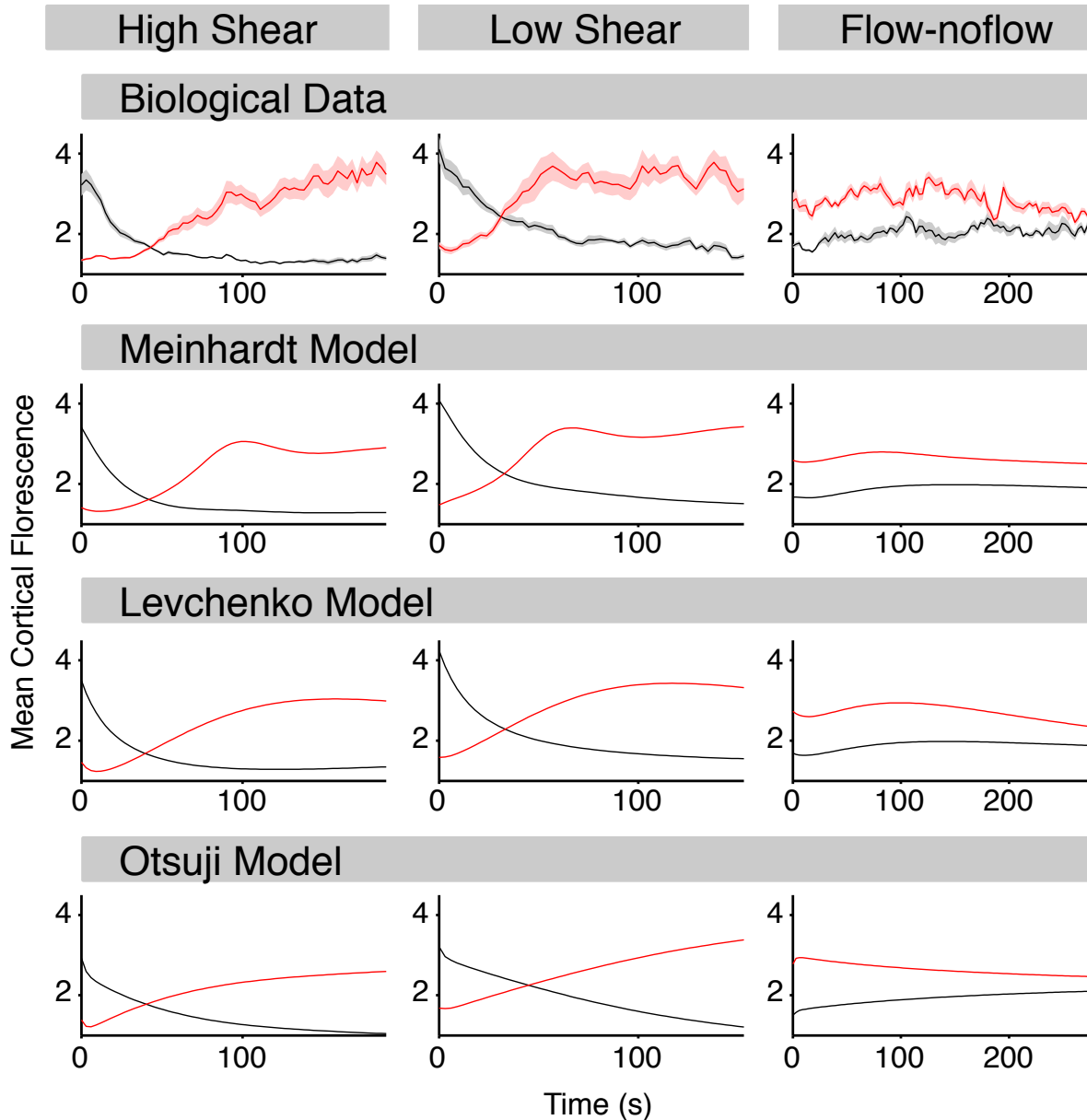


# Fitting the Meinhardt model to averaged time course data



# Simultaneous fitting of three experimental conditions

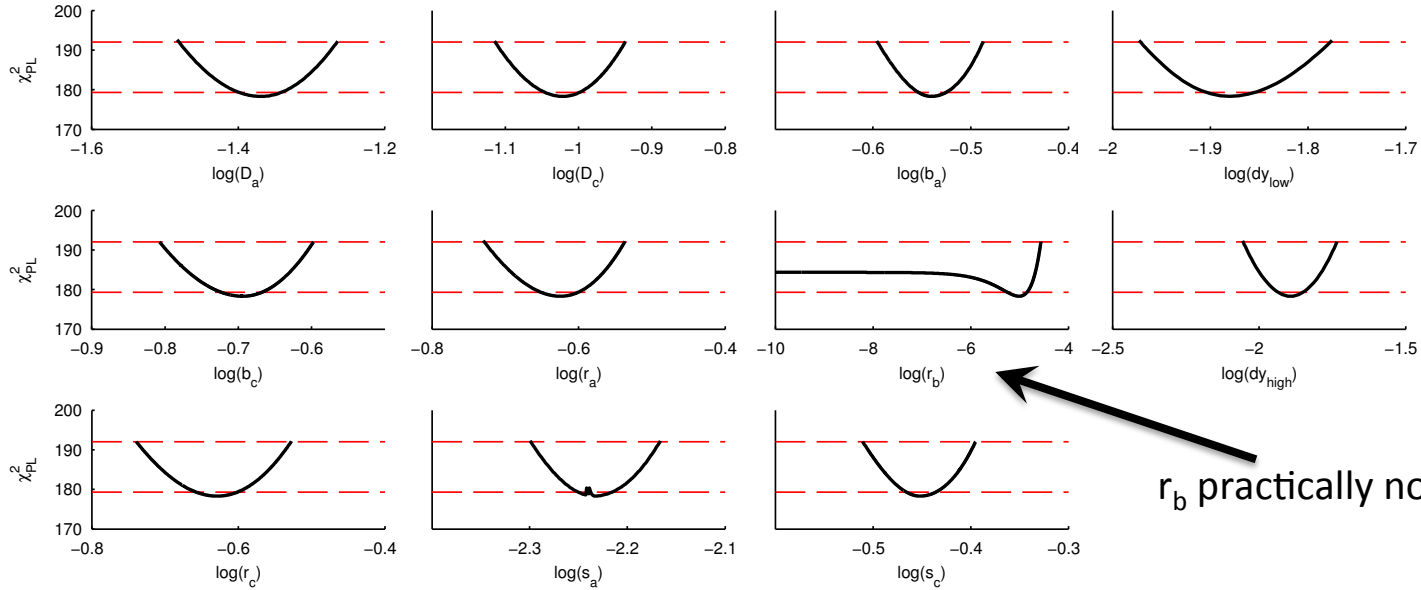
Red: emerging new front, black: linearly decaying old front



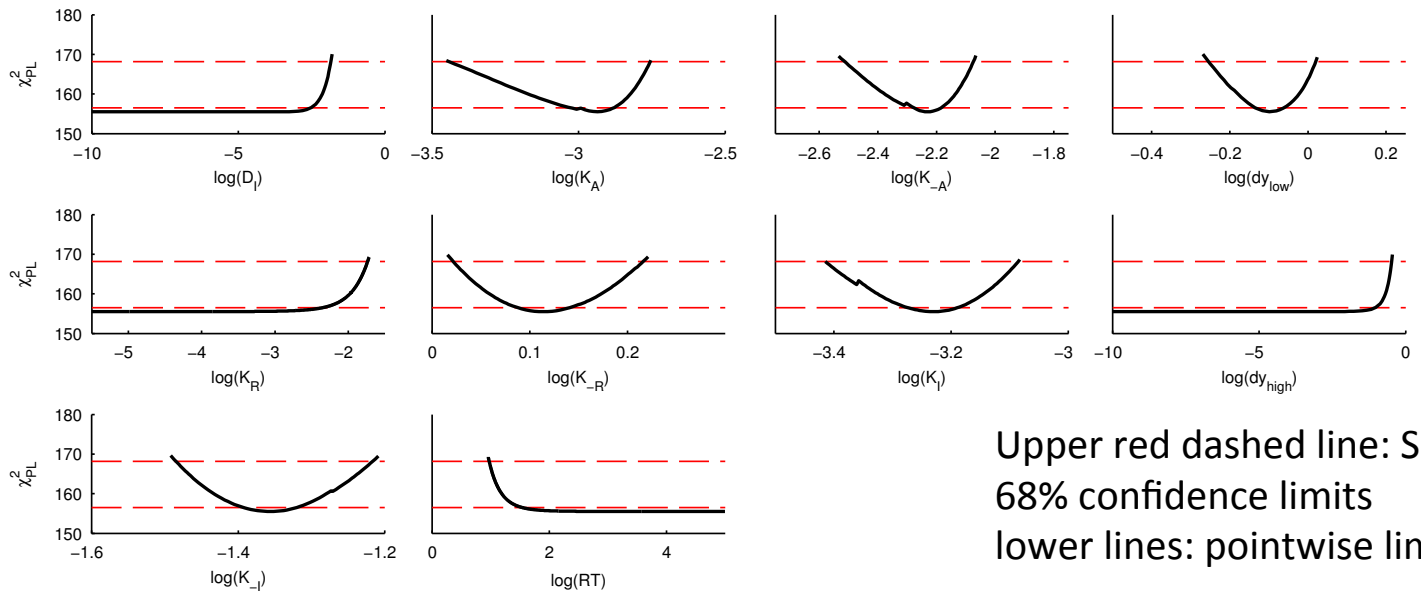


# Identifiability analysis: Profile likelihood estimation

Meinhardt Model



Levchenko Model



Upper red dashed line: Simultaneous 68% confidence limits  
lower lines: pointwise limits

## Reducing the Meinhardt model

- Inhibitor B turns out to stay almost constant
- replace it by  $B(P)=1+\beta_0(P^2 +\beta_1P)$  where P is the pressure in Pascal
- $dy(P=0) = 0$ , and  $dy(P) = \text{const}$

$$\frac{\partial A}{\partial t} = \frac{sr_a(\frac{A^2}{B} + b_a)}{(s_c + C)(1 + s_a A^2)} - r_a A + D_A \frac{\partial^2 A}{\partial x^2}$$

$$\frac{dB}{dt} = r_b \sum_n \frac{A}{n} - r_b B$$

$$\frac{\partial C}{\partial t} = b_c A - r_c C + D_C \frac{\partial^2 C}{\partial x^2}$$

$$s = (1 + dy \cos(2\pi x))$$

**original**

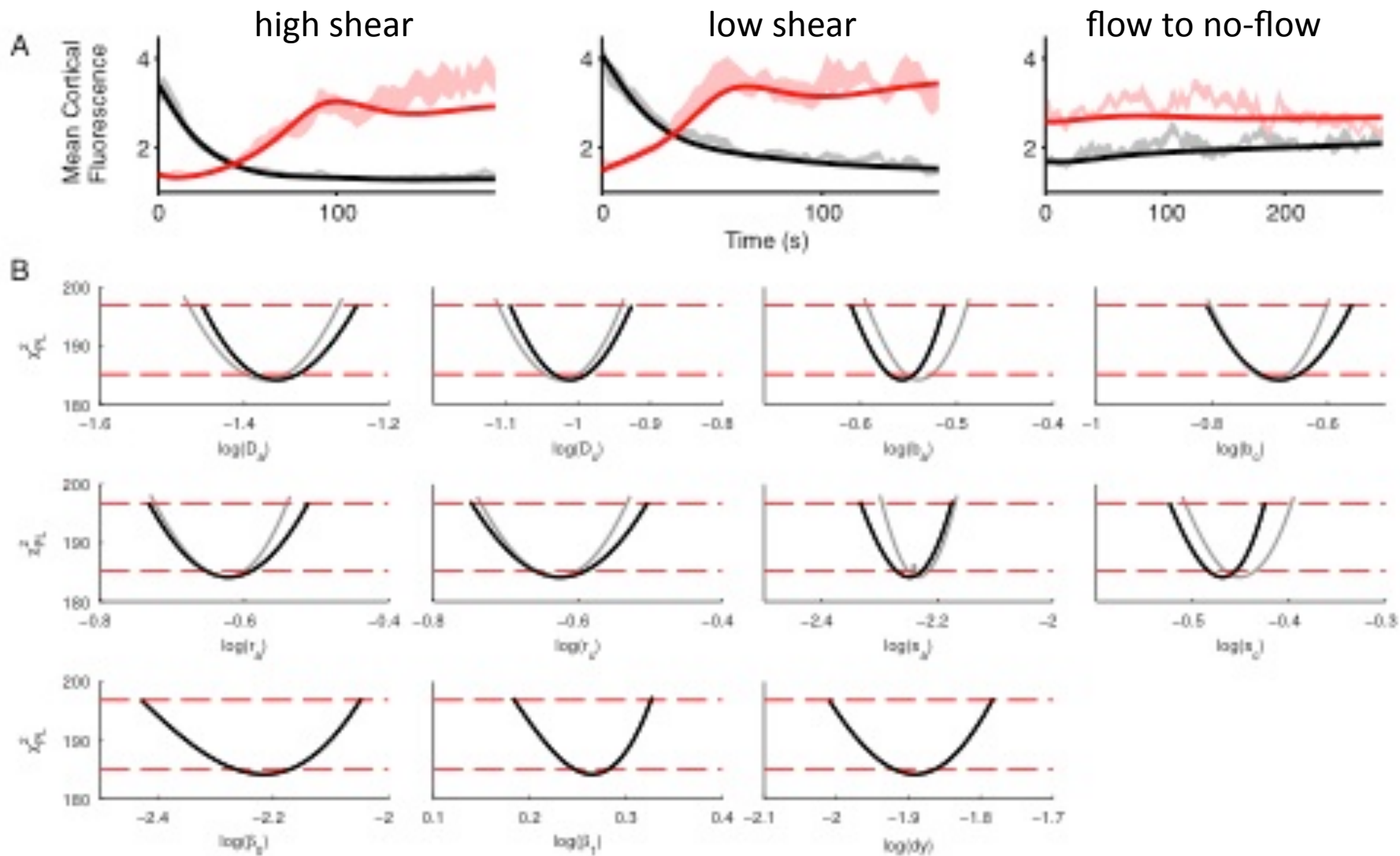
$$\frac{\partial A}{\partial t} = \frac{sr_a(\frac{A^2}{B(P)} + b_a)}{(s_c + C)(1 + s_a A^2)} - r_a A + D_A \frac{\partial^2 A}{\partial x^2}$$

$$\frac{\partial C}{\partial t} = b_c A - r_c C + D_C \frac{\partial^2 C}{\partial x^2}$$

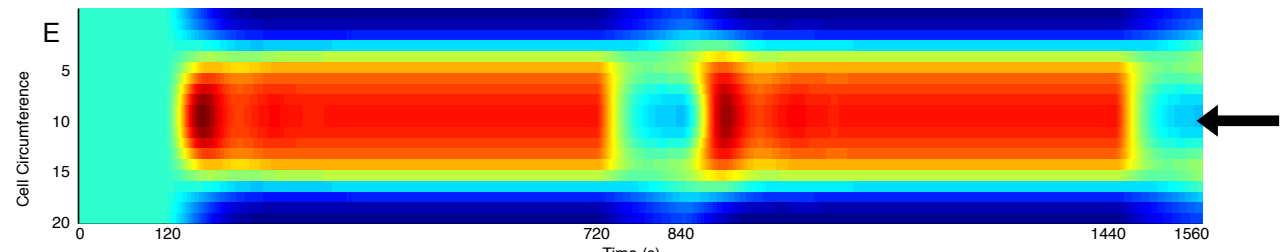
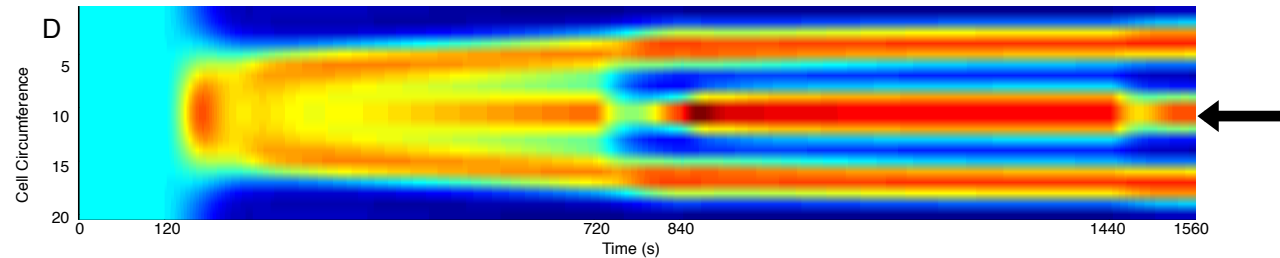
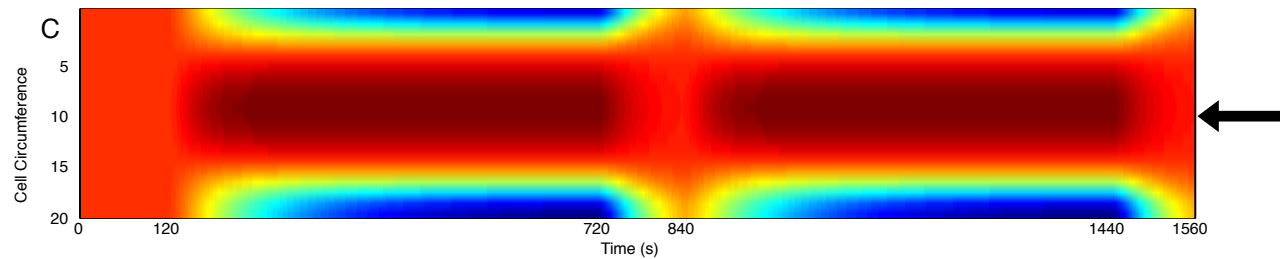
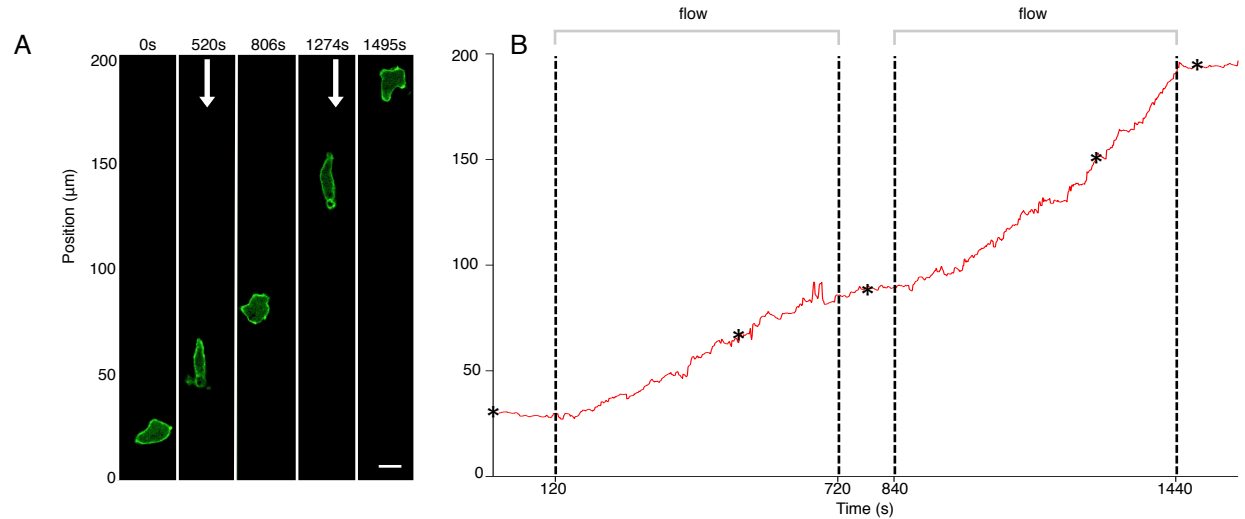
$$s = (1 + dy(P) \cos(2\pi x))$$

**modified**

# Removing inhibitor B from the Meinhardt model



# Making predictions: stable movement at P=1Pa



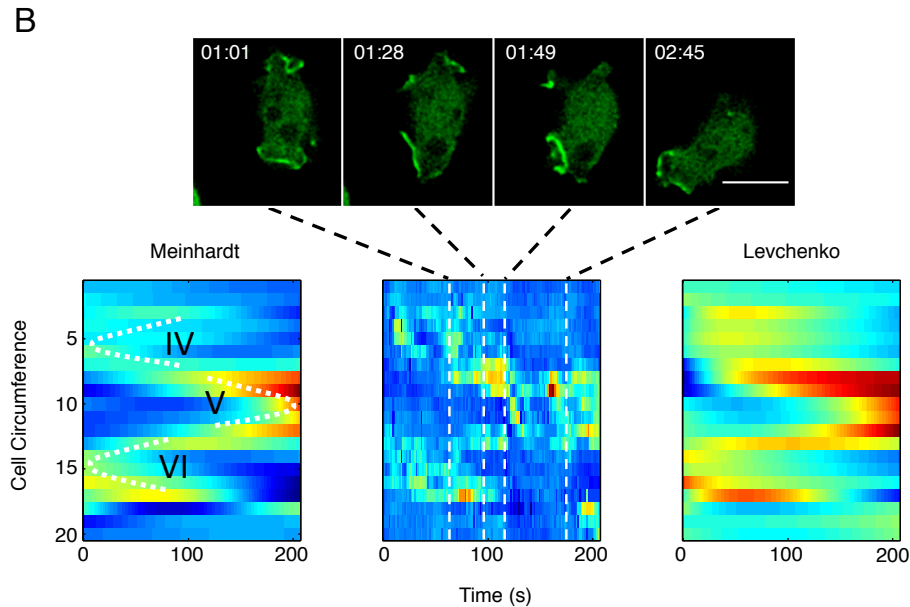
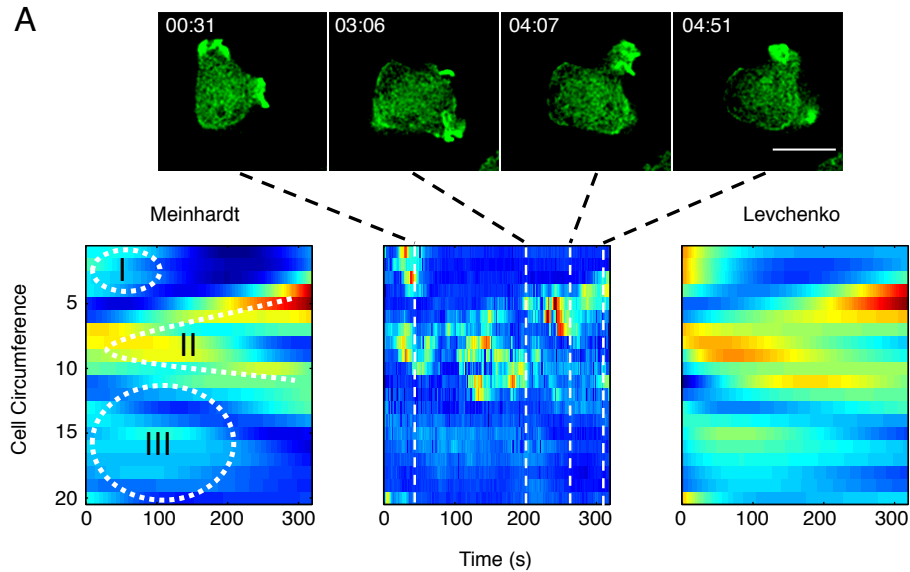
Levchenko  
(significant parameter  
change required)

2-variable Meinhardt  
(parameters as before:  
front splits in three)

2-variable Meinhardt  
with  $D_C$  decreased by 20%

# Fitting spontaneous movement of single cells

(convolution performed by deterministic PDE models helps interpreting the underlying stochastic process, estimating timescales of how determined a system actually is)



# Parameters

Original Meinhardt  
3-variable

Meinhardt 2-variable  
(identifiable)

Meinhardt 2-variable  
Single stable front

Meinhardt 2-variable  
Random motility

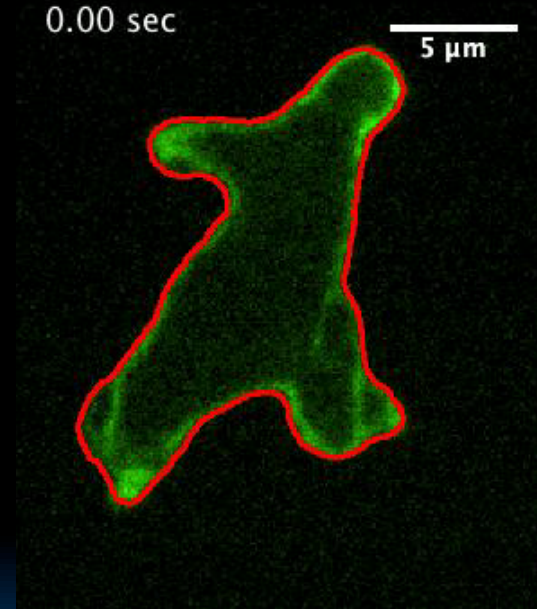
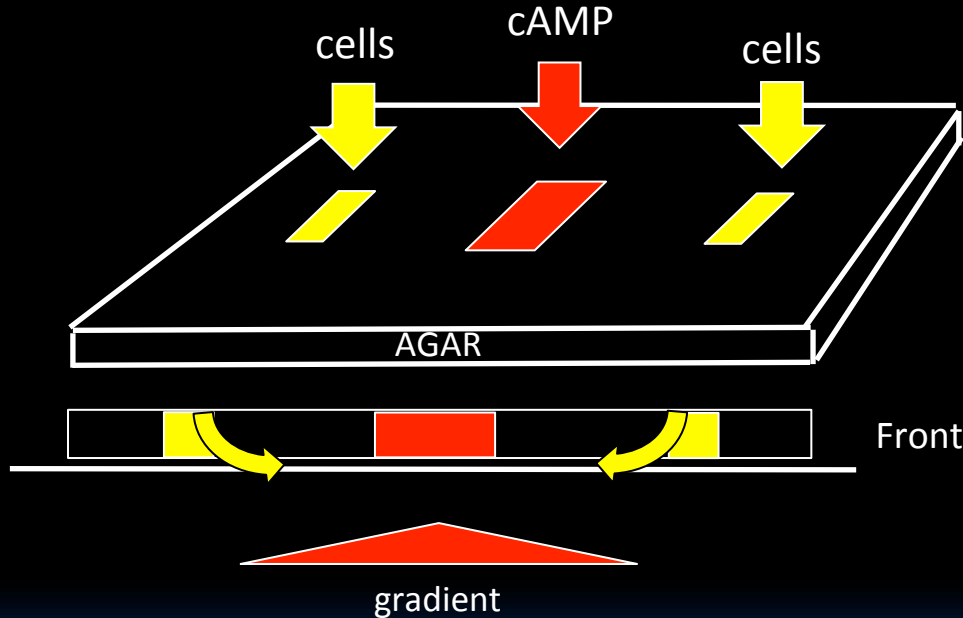
$D_A$	$4.274 \times 10^{-2}$	$D_A$	$4.415 \times 10^{-2}$	$D_A$	$4.415 \times 10^{-2}$	$D_A$	$2.311 \times 10^{-3}$
$D_C$	$9.513 \times 10^{-2}$	$D_C$	$9.768 \times 10^{-2}$	$D_C$	$7.064 \times 10^{-2}$	$D_C$	$1.471 \times 10^{-8}$
$b_a$	0.2881	$b_a$	0.2776	$b_a$	0.2776	$b_a$	0.1438
$b_c$	0.2022	$b_c$	0.2076	$b_c$	0.2076	$b_c$	$5.643 \times 10^{-2}$
$r_a$	0.2371	$r_a$	0.2393	$r_a$	0.2393	$r_a$	$9.467 \times 10^{-2}$
$r_c$	0.2346	$r_c$	0.2378	$r_c$	0.2378	$r_c$	$6.552 \times 10^{-2}$
$s_a$	$5.833 \times 10^{-3}$	$s_a$	$5.647 \times 10^{-3}$	$s_a$	$5.647 \times 10^{-3}$	$s_a$	$3.054 \times 10^{-3}$
$s_c$	0.3534	$s_c$	0.3397	$s_c$	0.3397	$s_c$	0.2791
$r_b$	$1.000 \times 10^{-5}$						
		$\beta_0$	$6.081 \times 10^{-3}$	$\beta_0$	$6.081 \times 10^{-3}$		
$dy_{low}$	$1.318 \times 10^{-2}$	$\beta_1$	1.840	$\beta_1$	1.840		
$dy_{high}$	$1.281 \times 10^{-2}$	$dy$	$1.280 \times 10^{-2}$	$dy$	$1.280 \times 10^{-2}$		

## Summary Reorientation

- Well-established tools (Potterswheel) for fitting systems of ODEs can be used to fit reaction-diffusion models. The most simple approach is based on a finite-difference discretization of the diffusion operator.
- Profile likelihood estimations helps immensely to evaluate the identifiability of models.
- Two popular models for cell orientation (Meinhardt and Levchenko) fit similarly well. A reduced version of the Meinhardt model is fully identifiable.
- Predictions help to further constrain parameters. Long term stability of single fronts can be achieved by a 20% reduction of  $D_C$ , the diffusion constant of the inhibitor.
- We are able to fit single cell data of randomly migrating cells. Because they need to produce simultaneous fronts, the derived parameter set is significantly changed.

# Migration under agarose induces blebbing in Dictyostelium

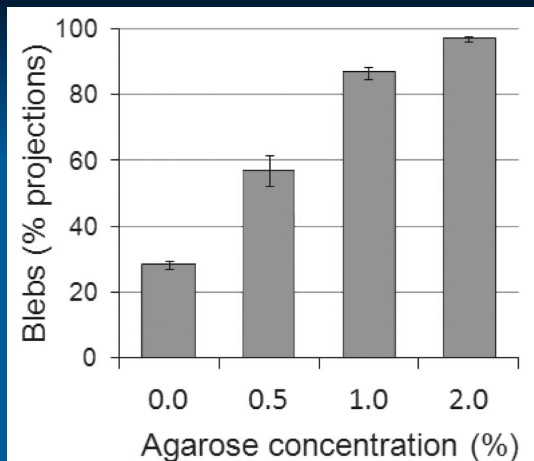
with Evgeny Zatulovskiy, Rob Kay  
(MRC LMB, Cambridge)



F-actin marker: GFP-ABD (ABP-120)

Spinning disk microscopy (4.5 fps)

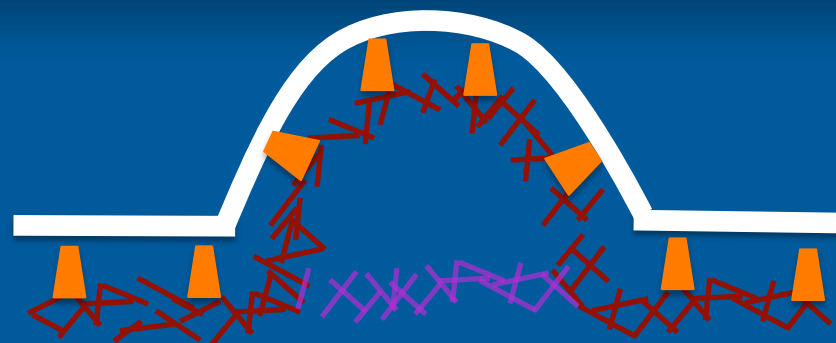
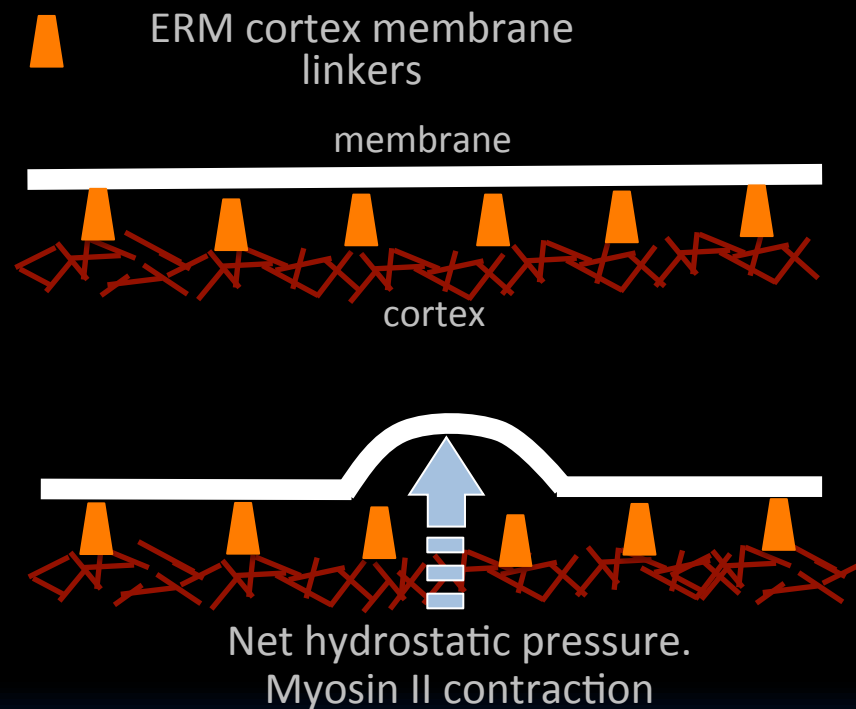
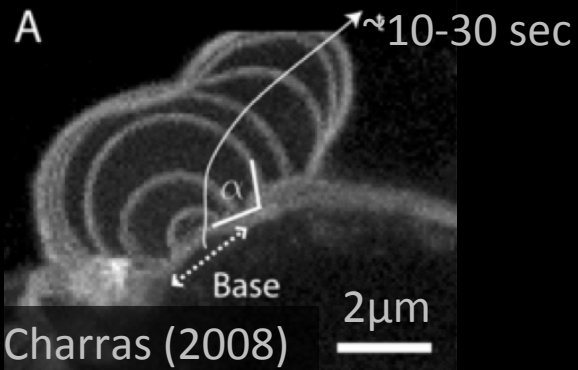
Confocal microscopy (2 fps)





# Blebbing is driven by Myosin-II dependent pressure

M2 melanoma cell line



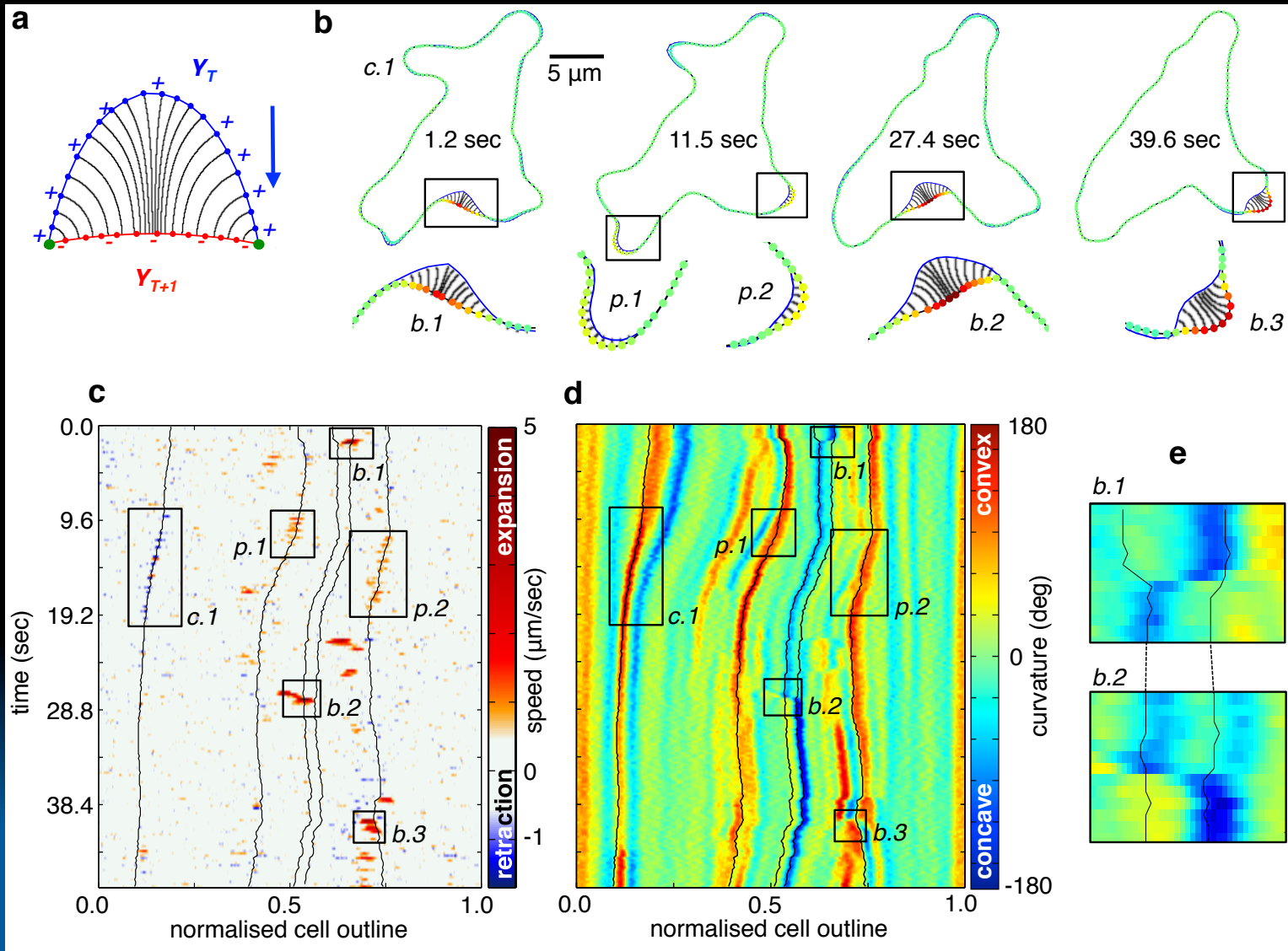
## Cellular blebbing

- Myosin-II dependent, driven by hydrostatic pressure
- Often found in cells moving in 3D constrained environments (zebrafish primordial germ cells, tumor cell migration)

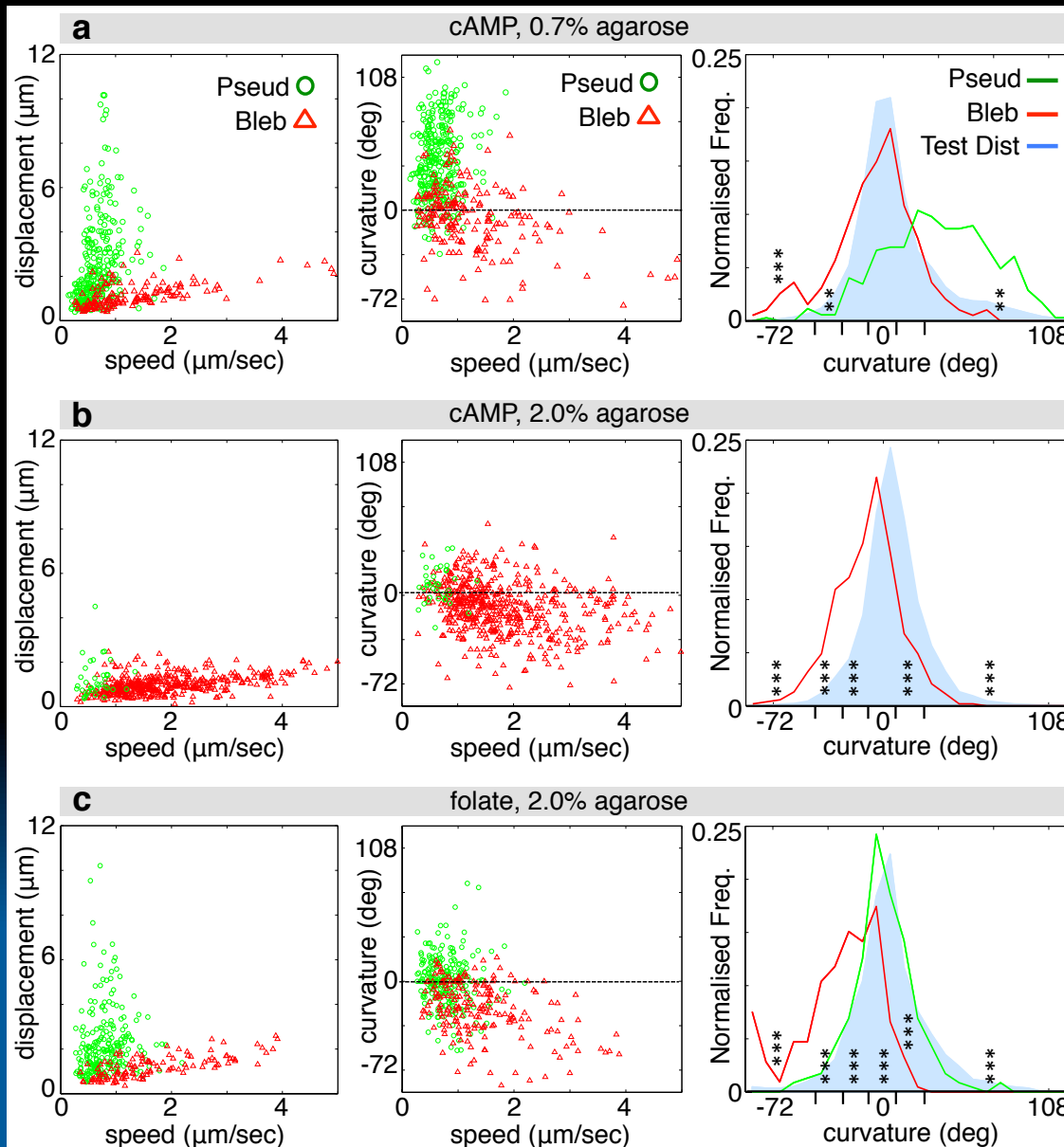
**How can cells direct blebs to the cell front? How do blebs and actin based protrusions interact?**

- Previously known regulators of bleb site selection:  
Weakening of the acto-myosin cortex, local contraction of myosin-II, asymmetric distribution of membrane-cortex linkers
- New: Cell geometry and membrane tension are important factors in bleb site selection, too

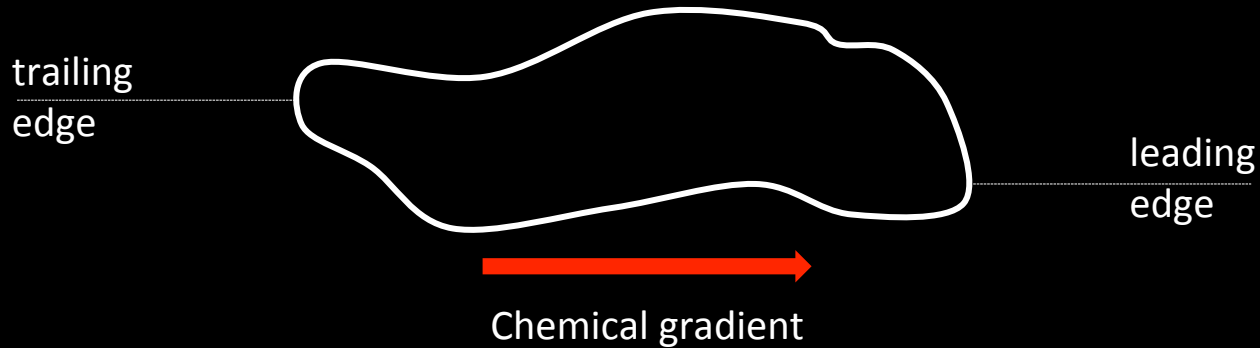
# ECMM-APT: Automatic Protrusion Tracking



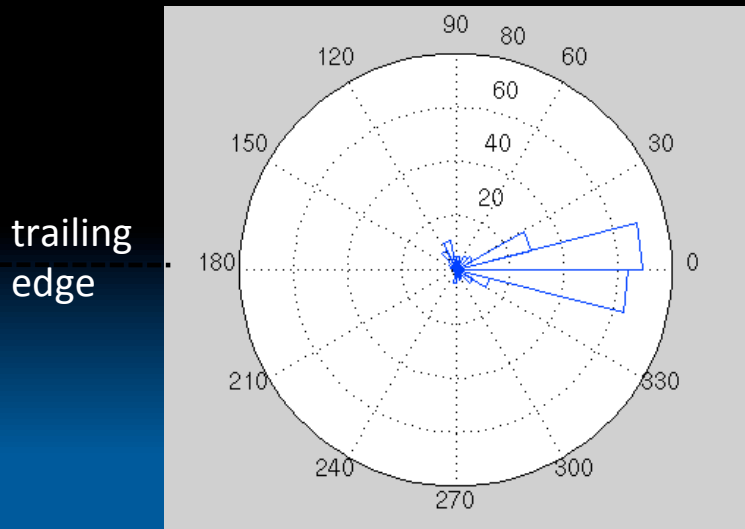
# Negative curvature promotes blebbing



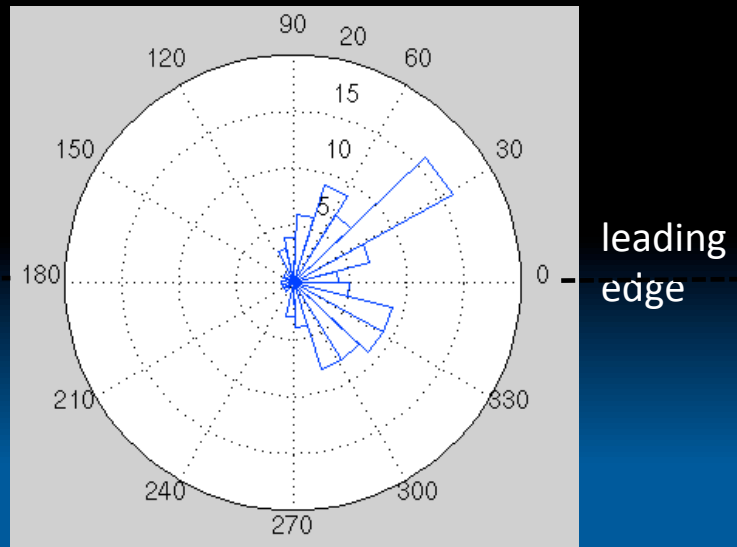
# Blebs Nucleate at the Flanks (Armpits) During Chemotaxis



### Frequency of Actin-driven Pseudopodia Nucleation

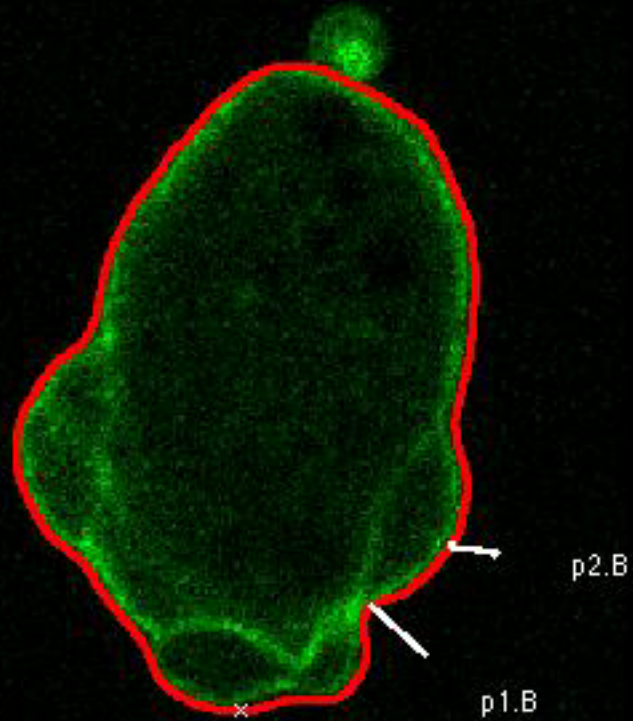


### Frequency of Bleb Nucleation



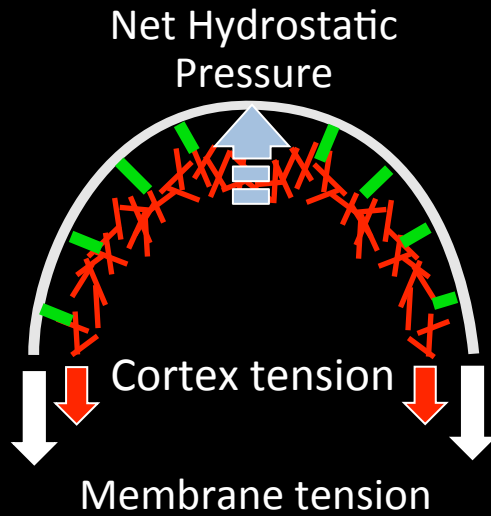
# Chains of blebs under 2% agarose (bleb only mode)

0.0 sec

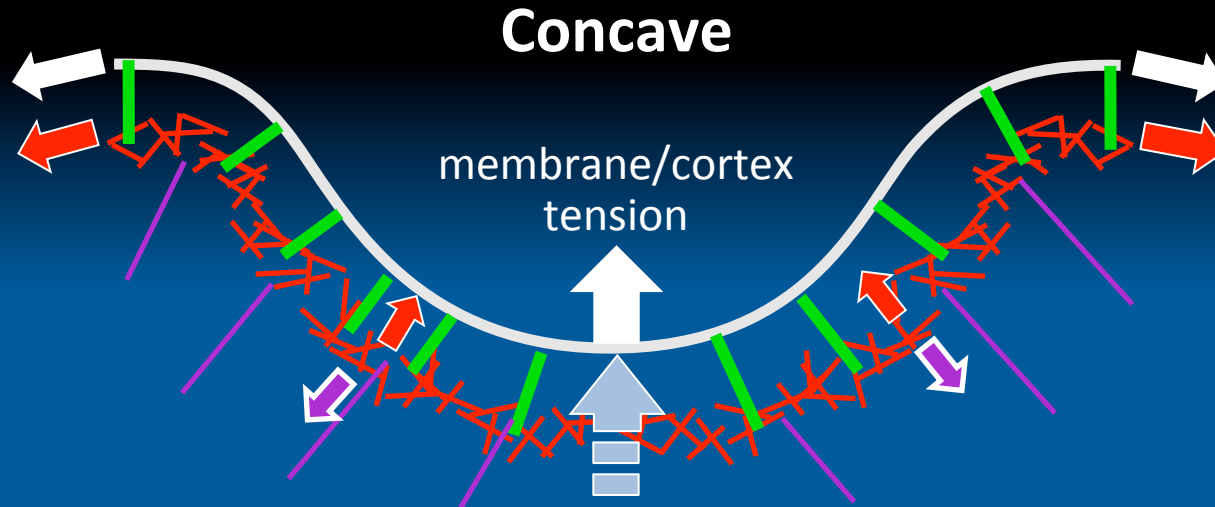
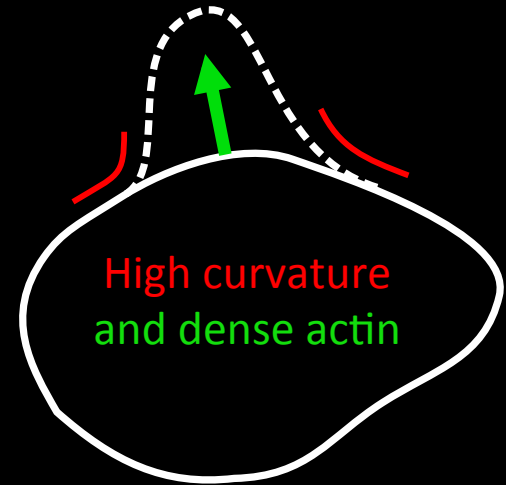


# Actin driven protrusions can localize bleb nucleation in *Dictyostelium*

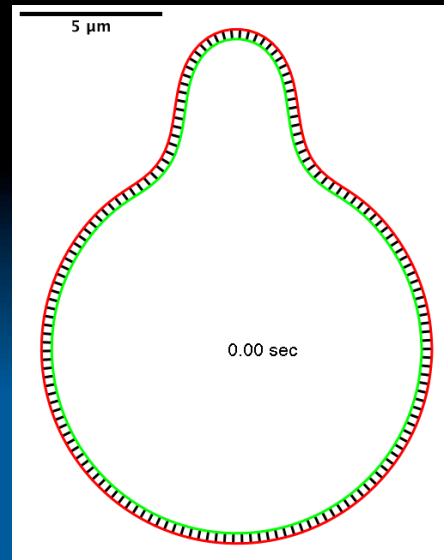
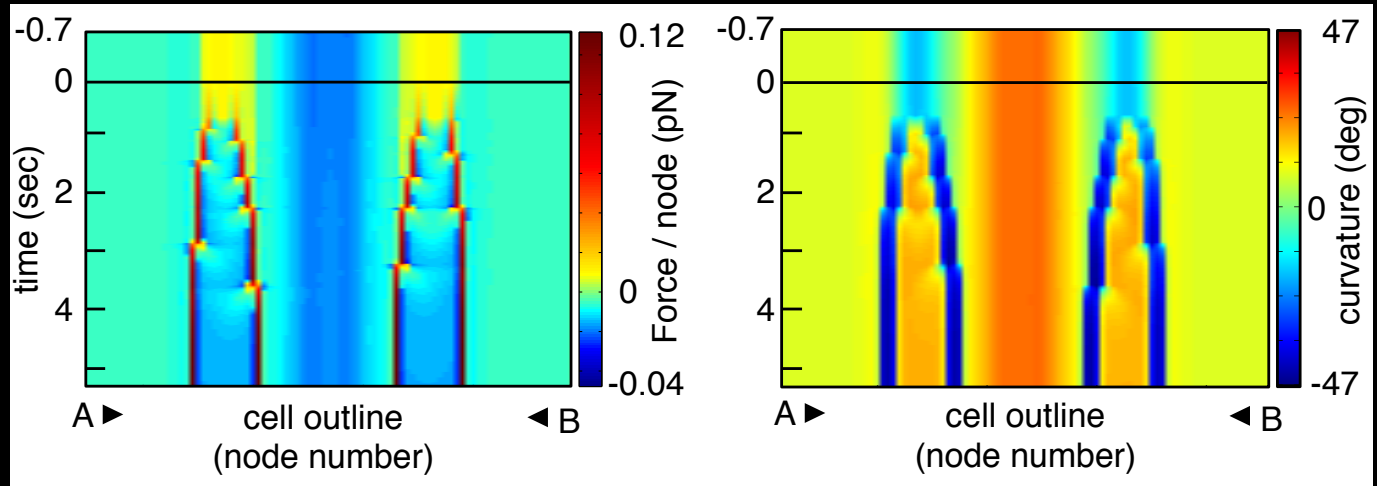
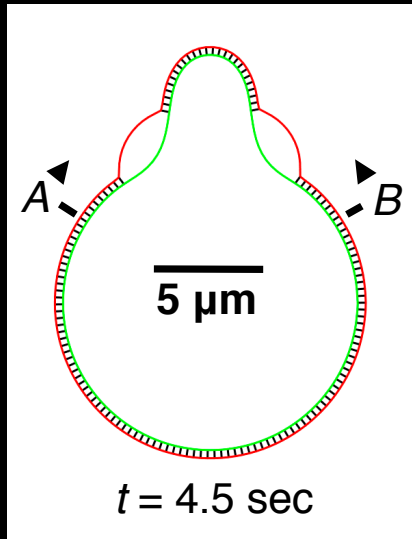
F-actin drives the formation of blebs by inducing curvature



Convex



# A biomechanical model for bleb initiation



**Forces:** Membrane tension, bending rigidity, intracellular pressure, Hookean springs link membrane and cortex. Linkers break above certain length.

Actin cortex is considered fixed during blebbing, no regrowth of actin cortex at the naked membrane.



# Blebbing of Fundulus deep cells maintaining a highly curved waist



## Summary Blebbing

Long term goal: Linking biochemistry and mechanics

- Actin provides a force pushing the cell membrane outward, and increases membrane tension. Work by Orion Weiner and others has shown that membrane tension quenches protrusive activity at the cell rear (long range inhibition). Our work shows that tension has a dual role: In concave regions it can also act as a local activator of cellular protrusions in form of blebs.

## Current members



**Richard Tyson**, QuimP,  
Blebbing in *Dictyostelium*



**Chengjin Du**, CellTracker:  
Quantifying transcription factor  
dynamics, 3D cell reconstructions



**Robert Lockley**, Modelling  
cell polarity



**Neil Venables**: Microtubule  
dynamics

## Alumni



**Mike Downey**, LineageTracker



**Ingrid Tigges**, Microfluidics  
experiments, now working for  
Mathworks

## Main Collaborators

Graham Ladds, Warwick Medical School  
Rob Kay, MRC-LMB, Cambridge  
Kees Weijer, University of Dundee  
Len Stephens, Babraham, Cambridge